

ภาคผนวก



# Carbon doped tungsten oxide nanorods NO<sub>2</sub> sensor prepared by glancing angle sputtering

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## A B S T R A C T

Metal oxide semiconductor nanostructures offer potential advantages in sensing applications due to their large surface to volume ratio, lower electron recombination rate, and high stability. However, most methods produce nanostructures with random sizes, distribution and orientations, which are not reliable for practical applications because of poor reproducibility. In this work, homogeneous carbon-doped WO<sub>3</sub> nanorods are developed based on the glancing angle deposition (GLAD) technique using radio-frequency magnetron sputtering and investigated for NO<sub>2</sub> gas sensing application. The carbon doping is achieved by using acetylene gas as a carbon source. Characterization based on scanning electron microscopy, Auger electron spectroscopy and X-ray diffraction confirm the formation of uniform carbon-doped crystalline WO<sub>3</sub> nanorods. The gas-sensing results reveal that carbon-doped WO<sub>3</sub> nanorods sensor exhibits not only high response and selectivity to NO<sub>2</sub> (0.5–5 ppm) but also at low operating temperature (150 °C) compared with the undoped ones. The observed gas-sensing enhancement may be attributed to the increase of specific surface area and the decrease of activation energy by carbon doping.

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## 1. Introduction

Nanostructures such as nanowires, nanorods, nanotubes of metal oxide semiconductor (MOS) materials have recently attracted monumental interest in gas-sensing applications because of their excellent performances owing to their large surface to volume ratio, lower electron recombination rate and high stability. Among various MOS materials, tungsten trioxide (WO<sub>3</sub>) is a highly promising candidate due to its fast response with high sensitivity toward NO<sub>x</sub> [1–4], H<sub>2</sub>S [5–8], C<sub>2</sub>H<sub>5</sub>OH [8,9], CO [10], NH<sub>3</sub> [10–14], [15] and H<sub>2</sub> [16]. Moreover, addition of some foreign atoms such as Pt, Pd, or Au [17–21] to WO<sub>3</sub> usually improves the sensitivity and selectivity to some particular gases. However, these additives are mostly expensive noble metals, which are not practical for low-cost applications. Recently, carbon based dopants have been reported as promising low-cost alternatives. For instance,

carbon nanotubes (CNTs) incorporation has been shown to be effective for improving sensitivity and selectivity toward H<sub>2</sub> of WO<sub>3</sub> thin film [22]. In another research, carbon doping provides considerable enhancement of toluene vapor sensitivity of WO<sub>3</sub> microtubes at low operating temperature [23].

WO<sub>3</sub> nanostructures have been fabricated based on a number of methods including thermal oxidization [24–26], spray pyrolysis [27], and chemical vapor deposition [28,29]. However, most methods produce nanostructures with random sizes, distribution and orientations, which are not reliable for practical applications because of poor reproducibility. Recently, some processes including e-beam lithography, nanolithography and template-growth techniques have been developed to realize well-ordered nanostructures. Nevertheless, they require either expensive instrumentation or complicated fabrication procedures. Simple and low cost methods for well-ordered nanostructure construction are more preferred in gas-sensing and other commercial applications.

Glancing angle deposition (GLAD) technique is a relatively new method for fabrication of well-ordered and sophisticated nanostructures i.e. nanorods, nanoblade and zigzag nanocolumns [30–33]. It is a modified physical vapor deposition process, in which substrate surface is rotated and tilted to an angle greater than 80° with respect to the normal of substrate surface or less than 10°

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with respect to the direction of vapor flux. The vapor molecules directed to the substrate will experience shadowing and limited surface diffusion condition leading to the formation of isolated nanostructures. With this technique, the shape, size and density of nanostructures can be well controlled by deposition parameters such as deposition angle, operating pressure, substrate temperature, deposition power, and so on. There have been few reports of  $\text{WO}_3$  nanorods fabricated by the GLAD technique using DC magnetron sputtering [34–36]. However, there has been no report of carbon-doped  $\text{WO}_3$  nanorods prepared by the GLAD technique using radio-frequency (RF) magnetron sputtering and its application in gas sensing. In this work, carbon-doped  $\text{WO}_3$  nanorods are fabricated by GLAD technique using RF magnetron sputtering and investigated for  $\text{NO}_2$  gas sensing application. In addition, its performances are comparatively studied with that of the undoped ones.

## 2. Experimental details

### 2.1. Fabrication of $\text{WO}_3$ nanorod-based gas sensors

$\text{WO}_3$  nanorod-based gas sensors were fabricated by the direct deposition of  $\text{WO}_3$  nanostructures onto prefabricated interdigitated electrodes on alumina substrates. Interdigitated electrodes were used to reduce the resistance of  $\text{WO}_3$  material. These electrodes were prepared by sputtering Cr (~50 nm) and Au (~300 nm) on alumina substrates with pre-patterned photoresist and lift-off process. The interdigitated Au electrodes have a sensing area of  $1 \text{ mm} \times 5 \text{ mm}$  and the interdigit spacing of  $100 \mu\text{m}$ . In addition,  $\text{WO}_3$  nanorods were also deposited on bare silicon substrates for structural characterization. Prior to deposition, silicon wafers and alumina substrates were pre-cleaned successively with acetone and isopropanol by ultrasonication, dried in nitrogen atmosphere and then loaded into the deposition chamber.

Carbon-doped and undoped  $\text{WO}_3$  nanorods were deposited by variable angle RF magnetron sputtering system as schematically illustrated in Fig. 1. A 3-inch tungsten disc with 99.995% purity (K.J. Lesker) was used as the sputtering target. The distance from the target to substrate center and the substrate rotation were fixed at 7 cm and 60 rpm, respectively. The chamber was evacuated by

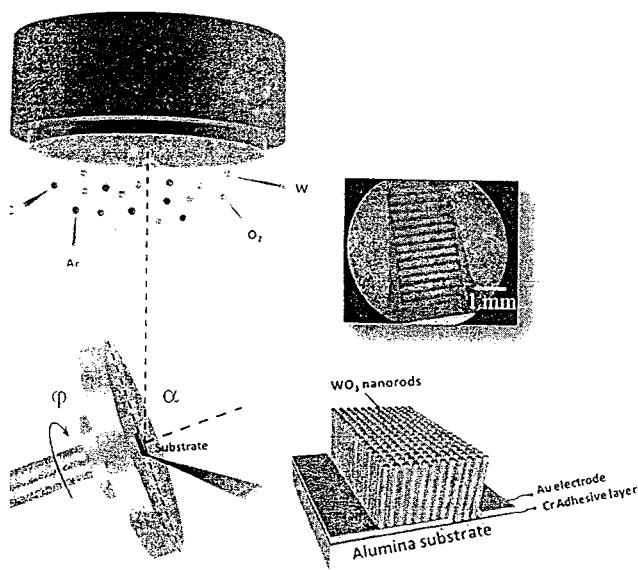


Fig. 1. Schematic of the carbon-doped  $\text{WO}_3$  nanorods array fabricated by the glancing-angle RF magnetron sputtering deposition. Inset shows photograph of Au electrode with sensing layer.

mechanical and turbomolecular pumps (Pfeiffer Inc.) while the vacuum pressure was continuously monitored with Pirani and Penning pressure gauges. For undoped  $\text{WO}_3$  nanorod deposition, W target was reactively sputtered in a mixture of 99.999% argon and 99.999% oxygen after a base pressure of  $5.6 \times 10^{-6}$  mbar. The flow rates of Ar and  $\text{O}_2$  were controlled with a mass flow controllers (MKS Inc.) at 9.6 and 11.0 sccm, respectively. The plasma discharge was generated at a constant RF power of 200 W at a sputtering pressure of  $5.0 \times 10^{-3}$  mbar for 3 h. The substrate normal was positioned at an angle of  $85^\circ$  ( $\alpha = 85^\circ$ ) with the respect to the vapor incident flux (the vertical axis). For carbon doping, 99.99% acetylene ( $\text{C}_2\text{H}_2$ ) as a carbon source was added at a flow rate of 1.1 sccm into the gas mixture and RF plasma was induced at a sputtering pressure of  $6.0 \times 10^{-3}$  mbar. The undoped and carbon-doped  $\text{WO}_3$  nanorods were then annealed in air for 3 h at  $400^\circ\text{C}$  to stabilize the crystalline structures. Photograph of the fabricated sensor is displayed in the inset of Fig. 1.

### 2.2. Characterization

The morphology, chemical composition and crystallographic structure of carbon-doped and undoped  $\text{WO}_3$  nanorods were characterized using a field emission scanning electron microscopy (FE-SEM, Hitachi S-4700), Auger electron spectroscopy (AES, EMSL 680), and X-ray diffraction (XRD, Rigaku Ttrax III). SEM and AES characterizations were conducted at an electron acceleration voltage of 10 kV. Prior to AES measurement, the surface of  $\text{WO}_3$  nanorods was sputtered to clean surface contamination by a 2 keV Argon ion beam for 1 min. Grazing-incidence XRD measurement was operated at 50 kV/300 mA with  $\text{Cu-K}\alpha_1$  radiation ( $\lambda = 1.54056 \text{ \AA}$ ). The detector scanning speed was set at a rate of  $1^\circ/\text{min}$  and the measurement was run from  $20$  to  $60^\circ$  incident angles in steps of  $0.02^\circ$ .

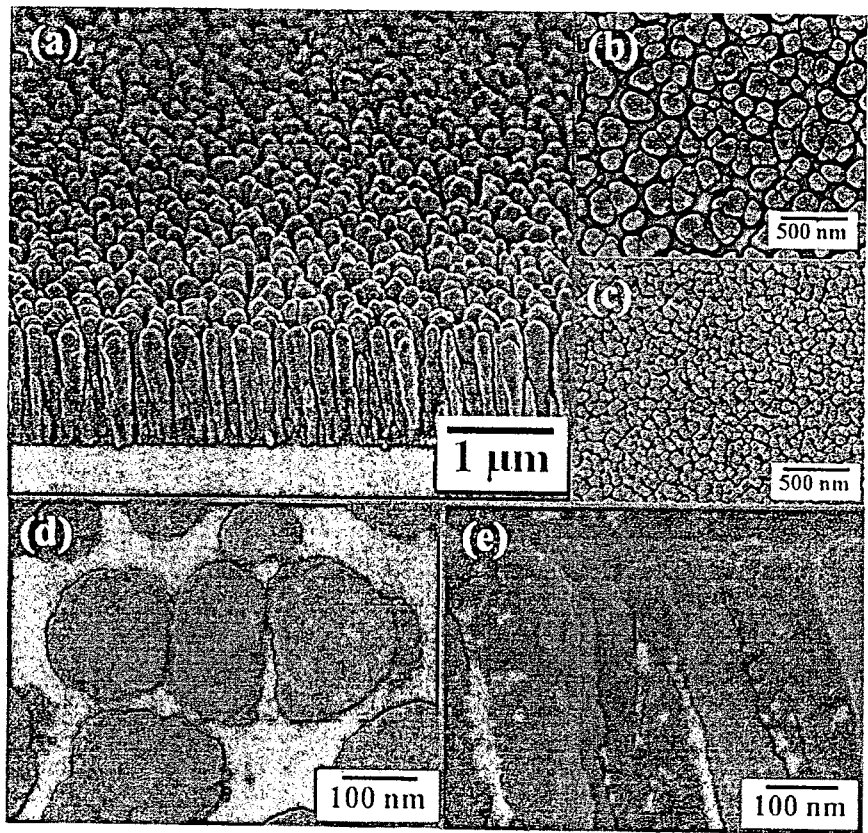
### 2.3. Gas sensing measurements

The gas sensing properties of the undoped and carbon-doped  $\text{WO}_3$  nanorods were measured using a dynamic flow system with gas concentrations controlled by using a mass flow controllers (Brook Instrument Inc.). A set of heaters made of Ni–Cr coils were used to supply a well-controlled operating temperature in the range of  $100$ – $300^\circ\text{C}$ . The sensors were tested by applying a constant voltage (10 V) and measuring electrical current using a 8846 A Fluke multimeter with 6.5 digit resolution. The resistance of gas sensors can be calculated from the simple Ohm's law. The target gases including nitrogen dioxide ( $\text{NO}_2$ ), hydrogen sulfide ( $\text{H}_2\text{S}$ ), hydrogen ( $\text{H}_2$ ), ammonia ( $\text{NH}_3$ ), carbon monoxide (CO), and ethanol (EtOH) vapor were introduced at various concentrations to assess the response and selectivity of the sensors. To avoid the humidity effects, the zero-grade dry air was used as the carrier gas. The times for response and recovery period were selected from the times to achieve at least 90% resistance change of the saturated value. The data were recorded every second using LabVIEW via a USB DAQ device for subsequent analyses.

## 3. Results and discussion

### 3.1. Characterization of structure and morphology

The surface morphologies of the as-grown products are displayed in Fig. 2. It can be seen that the glancing-angle RF magnetron sputtering deposition technique produces well-aligned  $\text{WO}_3$  vertical nanorods with highly uniform distribution over a large area (Fig. 2a). The nanorod structures results in a rougher surface and larger specific surface area compared to undoped ones. The average diameter (Fig. 2b) and length of carbon-doped  $\text{WO}_3$  nanorods are



2. FESEM images of (a) side view and (b) top view of carbon-doped WO<sub>3</sub> nanorods, (c) top view of undoped WO<sub>3</sub>, (d) and (e) partial wall-wall connections of nanorods.

mated to be ~174 nm and ~1.1 μm, respectively, corresponding n aspect ratio of ~6.3 while the undoped WO<sub>3</sub> nanorods have an age diameter of ~74 nm (Fig. 2c) and length of ~235 nm, lead-to an aspect ratio of ~3.2. It should be recalled that the time leposition for both structures were three hours. Thus, acety- : gas plays an important role in accelerating the growth of WO<sub>3</sub> orods, resulting in nanorod structure with higher aspect ratio. : phenomenon may be attributed to the enhancement of local istributive oxidation and temperature gradients and more details he carbon-assisted growth mechanism can be found in Ref. . From top-view SEM images at medium and low magnifica- s (Fig. 2b and c), nanorods seem to be isolated and connected ther only at their base. However, more detailed examination lustrated in Fig. 2d and e reveals that nanorods are partially ected along parts of their walls and the connection occurs inually throughout the nanorod array.

The growth mechanism of nanorods can be schematically illus- ed in Fig. 3. The vertically well-aligned WO<sub>3</sub> nanorods are ed due to the dominant of strong atomic self-shadowing under itions of limited adatom mobility [38–40]. The growth process e divided into two stages including (I) initial nucleation to a shadowing centers and (II) formation of columnar structures to the shadowing effect. Initially, deposited atoms are ran- ly distributed on a substrate forming initial nucleation sites. initial nucleated islands behave as the shadowing centers hide unoccupied sites and smaller islands from the incident or flux arriving at a glancing angle ( $\alpha = 85^\circ$ ). Thus, atoms from or flux only accumulate on taller islands, which are grown into ns. For materials with the limited adatom mobility such as , voids are not filled due to very slow surface diffusion [38]. efore, the layer consisting of nanorods is formed with sep- on of narrow pores. It should be noted that vapor flux can

be divided into vertical and lateral components with respect to substrate. However, the average lateral component becomes zero because of the cancelation of lateral component at opposite direc- tions under a constant-speed substrate rotation, leading to vertical growth [39].

Auger electron spectra of carbon-doped and undoped WO<sub>3</sub> nanorods are demonstrated in Fig. 4. The spectra contain only three existing elements including carbon, tungsten and oxygen.

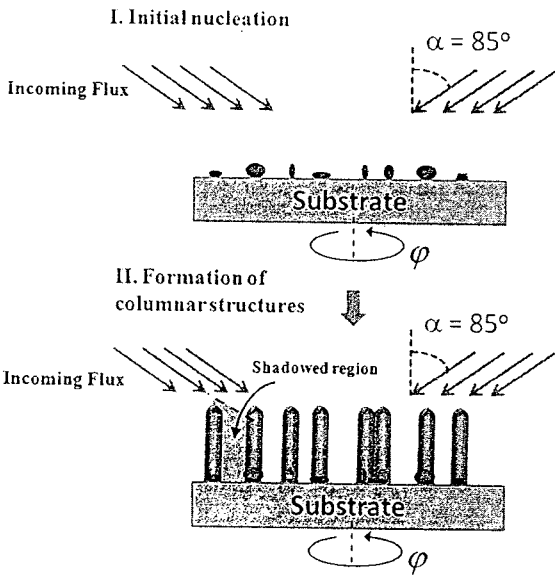


Fig. 3. Model of nanorods formation using GLAD technique.



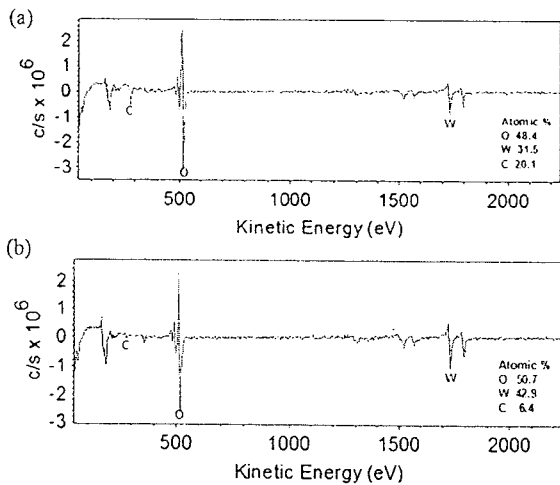


Fig. 4. Auger electron spectra of (a) carbon-doped and (b) undoped  $\text{WO}_3$  nanorods.

The spectrum of carbon doped sample shows apparently higher carbon peak than that of the undoped one and the carbon contents of carbon-doped and undoped are estimated to be 20.1 and 6.4 at% respectively. Thus, the result confirms that carbon is incorporated into  $\text{WO}_3$  nanorods and the produced nanorods have high purity without contamination from other elements. Fig. 5 shows XRD patterns of carbon-doped and undoped  $\text{WO}_3$  nanorods. Both carbon-doped and undoped  $\text{WO}_3$  nanorods can be well indexed to the standard pattern of monoclinic  $\text{WO}_3$  with lattice constants of  $a = 7.297 \text{ \AA}$ ,  $b = 7.539 \text{ \AA}$ , and  $c = 7.688 \text{ \AA}$  (JCPDS No. 43-1035). No peak of impurities is found in these XRD patterns. By using Scherrer equation, the average grain size based on the peak from  $21.5^\circ$  to  $5.5^\circ$  can be calculated to be 23 nm and 26 nm for the undoped  $\text{WO}_3$  nanorods and the carbon-doped  $\text{WO}_3$ , respectively. Therefore, carbon doping causes a small increase of grain size but does not change the crystallinity of the  $\text{WO}_3$  nanorods, which is in agreement with another report of C doping in  $\text{WO}_3$  films [41].

## 2. Gas sensing properties

The gas-sensing properties of the sensors are primarily characterized in terms of gas response. The gas response to reducing gases (i.e.  $\text{H}_2$ ,  $\text{NH}_3$ ,  $\text{CO}$ ,  $\text{H}_2\text{S}$ , EtOH) and to oxidizing gases (i.e.  $\text{NO}_2$ ) are defined as  $R_a/R_{\text{rg}}$  and  $R_{\text{og}}/R_a$ , respectively, where  $R_a$  is the resistance of sensor in pure air,  $R_{\text{rg}}$  is the resistance of sensor in reducing gas,

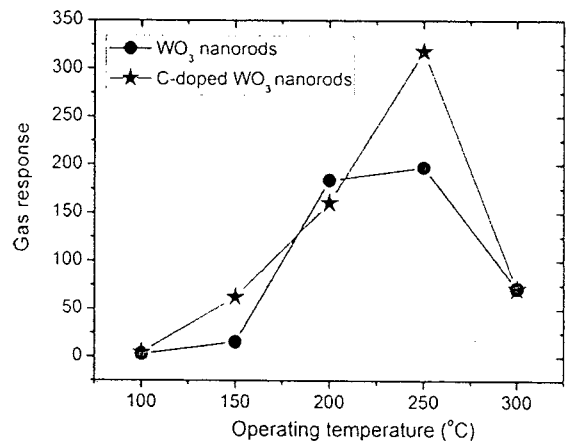


Fig. 6. Operating temperature dependence of gas responses to 3 ppm  $\text{NO}_2$ .

and  $R_{\text{og}}$  is the resistance of sensor in oxidizing gas. Fig. 6 shows the gas response of the C-doped and undoped  $\text{WO}_3$  nanorods gas sensors to 3 ppm  $\text{NO}_2$  at different operating temperatures. It can be seen that the gas responses of both gas sensors increase with increasing operating temperatures from  $100^\circ\text{C}$  to  $250^\circ\text{C}$  and then decrease as the operating temperature increases further. Thus, the optimum operating temperature of both nanorods gas sensors are around  $250^\circ\text{C}$ . In general, the increase of operating temperature contributes to the increase of the adsorption, diffusion and surface reaction rates [22,42]. In other words, sufficient thermal energy helps the reactions involved overcome their respective activation energy barriers leading to increase sensor response with increasing operating temperatures from  $100^\circ\text{C}$  to  $250^\circ\text{C}$ . However, desorption process will dominate and the diffusion depth becomes lower when operating temperature becomes too high leading to the decrease of gas response [43]. This behavior can also be well explained by the diffusion theory [44].

Dynamic response of the carbon-doped and undoped  $\text{WO}_3$  nanorods gas sensors toward  $\text{NO}_2$  at the optimum operating temperature of  $250^\circ\text{C}$  is illustrated in Fig. 7. It can be seen that both carbon-doped and undoped  $\text{WO}_3$  nanorods behave as  $n$ -type semiconductors since the sensor's resistances increase upon the introduction of oxidizing  $\text{NO}_2$  gas. In addition, the resistance of carbon-doped  $\text{WO}_3$  nanorods is more than an order of magnitude lower than that of undoped one, indicating a significant increase

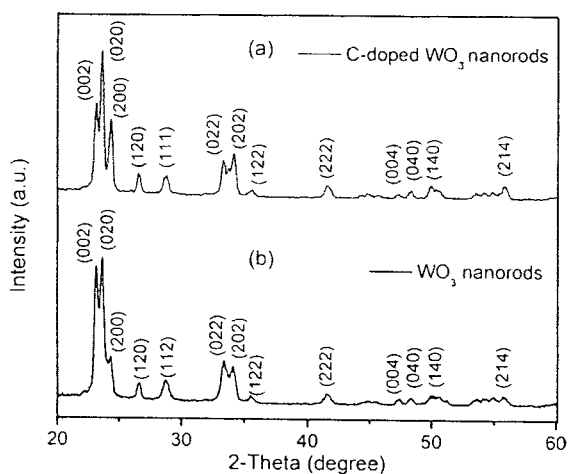


Fig. 5. XRD patterns of (a) carbon-doped and (b) undoped  $\text{WO}_3$  nanorods.

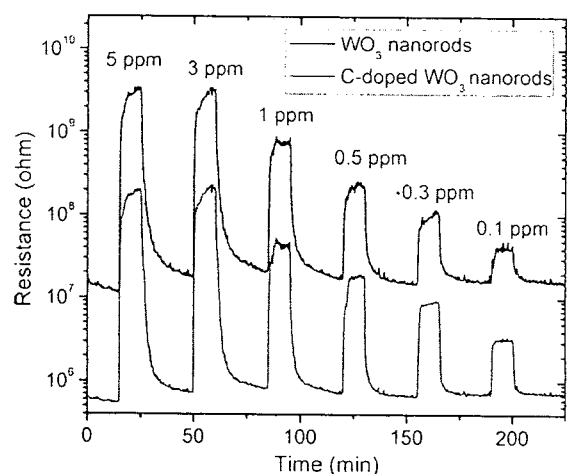


Fig. 7. Dynamic resistance response of the carbon-doped and undoped  $\text{WO}_3$  nanorods gas sensors toward  $\text{NO}_2$  based on optimum operating temperature of  $250^\circ\text{C}$ .

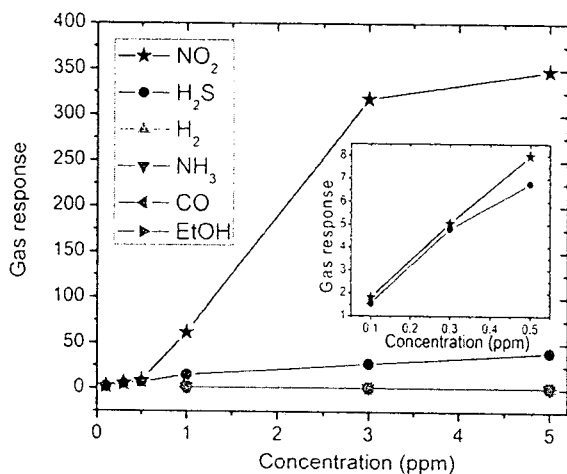


Fig. 8. Gas responses of carbon-doped WO<sub>3</sub> nanorod gas sensor versus concentration of different gases. The inset shows the gas responses at low concentrations of NO<sub>2</sub> and H<sub>2</sub>S ranging from 0.1 ppm to 0.5 ppm.

charge carrier concentration due to carbon incorporation. However, the sensors exhibit fast and stable response toward NO<sub>2</sub>. Response and recovery times are increased with increasing concentrations. The response times of the carbon-doped and undoped WO<sub>3</sub> nanorods gas sensors to 0.1 ppm NO<sub>2</sub> are estimated to be 17 s and 21 s, respectively while the corresponding recovery times are 50 s and 69 s. The improved response rate by carbon doping may be attributed to increased adsorption and desorption of NO<sub>2</sub> molecules on the WO<sub>3</sub> surface due to the increase of charge carriers.

In order to investigate the response and selectivity of C-doped WO<sub>3</sub> nanorods gas sensor, the sensor was exposed to NO<sub>2</sub>, H<sub>2</sub>S, H<sub>2</sub>, NH<sub>3</sub>, CO, and EtOH at various concentrations. Various gas responses of carbon-doped WO<sub>3</sub> nanorod sensor at the optimum operating temperature of 250 °C are displayed in Fig. 8. It can be seen that carbon-doped WO<sub>3</sub> nanorod sensor exhibits high response to NO<sub>2</sub> and is almost insensitive to H<sub>2</sub>, NH<sub>3</sub>, CO, and EtOH at concentrations ranging from 1 ppm to 5 ppm. At the concentration of 5 ppm, the response of carbon-doped WO<sub>3</sub> nanorod sensor to NO<sub>2</sub> and H<sub>2</sub>S is ~348 and ~40. Thus, the sensor clearly shows the selectivity to NO<sub>2</sub> at concentrations ranging from 1 ppm to 5 ppm. However, the response of sensor to NO<sub>2</sub> and H<sub>2</sub>S are not significantly different in the low concentration range (0.1 and 0.3 ppm, inset of Fig. 8). The detection limit of NO<sub>2</sub> for carbon-doped WO<sub>3</sub> nanorods sensor is estimated to be <0.5 ppm at the operating temperature of 250 °C. From Fig. 6, it can also be noticed that carbon-doped WO<sub>3</sub> nanorods gas sensor exhibits relatively high NO<sub>2</sub> response as compared to the undoped one at low operating temperature of 150 °C. It is useful to evaluate its response at low operating temperature (150 °C) for low-power gas-sensing applications. Fig. 9 shows gas responses of carbon-doped and undoped WO<sub>3</sub> nanorods gas sensors to NO<sub>2</sub> at various gas concentrations. It is evident that the gas responses of carbon-doped WO<sub>3</sub> nanorods sensor are considerably higher than those of the undoped sensor at all NO<sub>2</sub> concentrations. At a concentration of 5 ppm, the gas response of carbon-doped WO<sub>3</sub> nanorods sensor is ~114, which is ~2 times higher than that of undoped WO<sub>3</sub> nanorods sensor (~52). The enhancement of gas response at low operating temperature after carbon doping may be explained as follows. It was found that carbon doping results in the decrease of sensors resistance at 150 °C from 128 MΩ to 1 kΩ. This may imply the decrease of activation energy barrier for charge carrier generation. At low operating temperature, the undoped sensor exhibits low conductivity and low gas response because thermal energy is not enough to overcome the activation

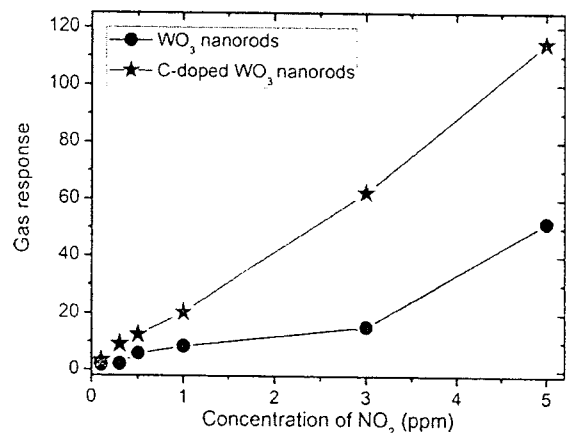


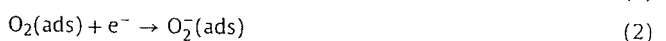
Fig. 9. Gas responses of carbon-doped and undoped WO<sub>3</sub> nanorods gas sensors to different concentrations of NO<sub>2</sub> at the operating temperature of 150 °C.

energy barrier. After carbon doping, the activation energy is reduced and charge carrier can be better thermally activated leading to higher gas response. In addition, the WO<sub>3</sub> nanorods sensor prepared by this method can detect NO<sub>2</sub> at relatively low operating temperature with high gas response compared to some other methods. For example, gas response to 1 ppm NO<sub>2</sub> of our carbon-doped WO<sub>3</sub> nanorods sensor is 18.2 at operating temperature of 150 °C while gas responses of WO<sub>3</sub> nanorods sensors prepared by thermal evaporation [25] and hydrothermal process [45] at their optimum operating temperature of 300 °C were reported to be 7 and 5.3, respectively.

### 3.3. Sensing mechanism

Based on the observation of FE-SEM (see Fig. 2d and e), nanorods connect together not only at their base but also along some parts of their sidewall. This allows current to flow from one electrode to another electrode with contribution of partial wall-wall nanorods connections as schematically illustrated in a simplified model (Fig. 10a). Thus, the sidewalls of WO<sub>3</sub> nanorods can also contribute to gas-sensing, leading to a large active gas-sensing area and high gas response. This is in agreement with the observed high NO<sub>2</sub> response (300–400), which should not be possible if only base of nanorods takes part in gas-sensing.

From the results, doping of carbon into WO<sub>3</sub> nanorods does not change the crystallinity but it tends to decrease activation energy and alter the thickness of the depletion layer. Sensing mechanism of carbon-doped WO<sub>3</sub> nanorods sensor may therefore be explained based on the model of general WO<sub>3</sub> nanorod sensor [43,46]. The sensing mechanism of NO<sub>2</sub> reactions on the surface of a single C-doped WO<sub>3</sub> nanorod is displayed in Fig. 10b. Initially, oxygen molecules from air adsorb on the surface of C-doped WO<sub>3</sub> nanorods and transform to chemisorbed oxygen species (O<sup>2-</sup>, O<sub>2</sub><sup>-</sup>, and O<sup>-</sup>) by trapping the electrons at the surface according to the following reactions [47]:



At the operating temperature of 100–300 °C, the chemisorbed oxygen species, O<sup>-</sup>, is known to be dominant. When O<sup>-</sup> species adsorb on surface, a depletion layer known as the space charge layer is formed at grain boundaries near the carbon-doped WO<sub>3</sub> nanorod surface. When a carbon-doped WO<sub>3</sub> nanorod is exposed to NO<sub>2</sub>,

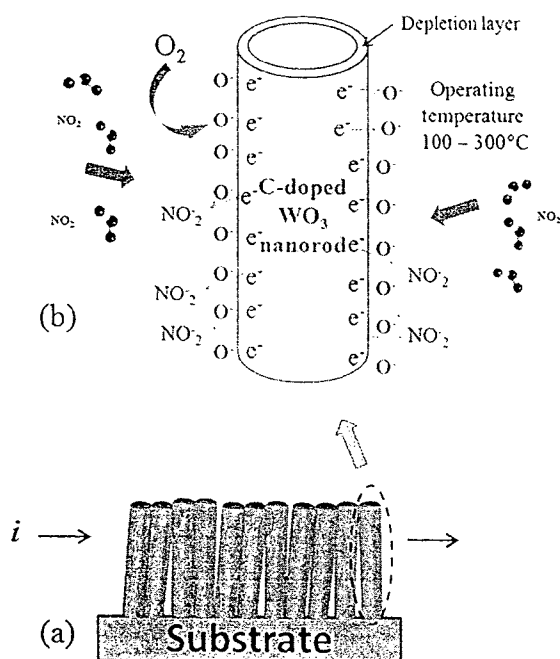
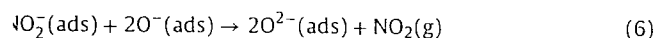


fig. 10. (a) Simplified model of a current flow through WO<sub>3</sub> nanorods from left side to right side and (b) Model of NO<sub>2</sub> reaction on the C-doped WO<sub>3</sub> nanorod surface.

NO<sub>2</sub> molecules directly adsorb on the surface of nanorods because NO<sub>x</sub> molecules own very high electron affinity (2.28 eV) compared with oxygen's value of 0.43 eV [48,49]. Moreover, the products from the reaction between NO<sub>2</sub> and e<sup>-</sup> on the surface also react with the O<sub>2</sub><sup>-</sup> species, resulting in the continuously decreasing concentration of electrons on the surface. The process can be described by the following reactions [50]:



The above reactions decrease the electrons from carbon-doped WO<sub>3</sub> nanorods and increase the thickness of the depletion layer, leading to the increase in resistance of carbon-doped WO<sub>3</sub> nanorods sensor.

## 1. Conclusion

Carbon-doped and undoped WO<sub>3</sub> nanorods gas sensors have successfully been fabricated by the GLAD technique with RF magnetron sputtering. By this technique, the vertically well-aligned homogeneous WO<sub>3</sub> nanorods with very low defect were achieved over a large area. It was found that carbon doping does not change the crystalline structure but increases the grain size and accelerates the nanorods growth leading to relatively high aspect ratios as compared to the undoped one. The fabricated carbon-doped WO<sub>3</sub> nanorods sensor exhibits high response and selectivity to NO<sub>2</sub> at the concentration range of 0.5–5 ppm at an optimum operating temperature of 250°C. In addition, the carbon-doped sensor still works well for NO<sub>2</sub> detection at lower operating temperature of 50°C due to the decrease of activation energy and alteration of the depletion layer. Therefore, carbon-doped well-ordered WO<sub>3</sub> nanorods with improved NO<sub>2</sub> gas-sensing performances in terms of response, response time, selectivity and operating temperature has been realized. Moreover, our technique offers distinct advantages over other methods such as high productivity, simplicity and low cost for well-ordered nanostructure construction.

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## Electronic Nose for Toxic Gas Detection based on Photostimulated

### Core-Shell Nanowires

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### Abstract

A novel fabrication of microelectronic nose based on ZnO nanowires and ZnO surface modifications including ZnO-ZnAl<sub>2</sub>O<sub>4</sub> core-shell nanowires and ZnO-Zn<sub>2</sub>TiO<sub>4</sub> core-shell nanowires gas-sensing elements operated at room temperature is reported. By combining vapor-phase transport processes and atomic layer deposition techniques, highly homogeneous core-shell nanowires structures can be successfully obtained on large scale areas. Under ultraviolet illumination on the specific oxide surfaces, photo-stimulated oxygen species ( $O_2^-(ads)$ ) response and dominate the gas sensing mechanism of the core-shell nanowire at room temperature. Principal component analysis results show the perfect discrimination of gases including toxic gases and non-toxic gases. This novel device can be used to identify both the gas type and the concentration of the gases with concentrations in the ppb level at room temperature.

**Keywords:** E-nose, Gas Sensor, 1D Nanostructures, ZnO, Kirkendall Effect

## 1. Introduction

Since more than a decade, so-called electronic noses (E-noses) became a very well-known practical device for sensing technology. With the ability to identify many detecting substances, E-noses are now widely used in several branches of science and engineering, for examples, biosensor E-nose, gas sensor E-nose, or liquid sensor E-nose [1-5]. Although originally it was created in analogy to 'a nose', the application of E-nose is far better than a natural nose in term of quantity analysis. Furthermore E-nose can be used to characterize a substance which might endanger humans.

A normal E-nose is composed of an array of sensors which usually has thin films as sensing receptors. Recently instead of using thin films, E-noses based on nanowires are in the focus of attention. The superior properties in 1D-nanostructure such as a higher surface per volume ratio, potential band-depletion, and surface charge accumulation can provide a better sensitivity with lower power consumption [6]. Therefore, attempts to produce nanowire based E-noses have been increasing. In order to fabricate nanowire sensor arrays, sets of sensors based on different materials are normally combined. An example was shown for instance by Chen et al. [7]. Carbon nanotubes,  $\text{In}_2\text{O}_3$ ,  $\text{SnO}_2$  and  $\text{ZnO}$  nanowires were used to act as different selective sensing material on the same E-nose platform. Baik et al. demonstrated a method to obtain an E-nose from a single material, i.e.  $\text{SnO}_2$  nanowires, with different metallic decorations on the surface [8]. Despite of the progress accomplished most of nanowire E-nose still requires high operating temperatures ( $>200^\circ\text{C}$ ). In this paper, we report the development of photo-stimulated E-noses based on pristine  $\text{ZnO}$  nanowires and surface reconstruction of  $\text{ZnO}$  nanowires including  $\text{ZnO-ZnAl}_2\text{O}_4$  core-shell and  $\text{ZnO-Zn}_2\text{TiO}_4$  core-shell nanowires that work at room temperature



for detecting toxic gases. The sensing mechanism of the core-shell nanowires under photo-activation will be discussed in details.

## 2. Experimental details

The fabrication of the respective ZnO NW based E-nose started with the preparation of a 100 nm dry oxide ( $\text{SiO}_2$ ) as insulated layer on a Si wafer accomplished in the usual way. The Cr (5 nm): Au (100 nm) interdigitated electrode array (IDA) with comb-like pattern was then fabricated on the insulator by conventional photolithography. The produced IDA was cleaned with acetone, isopropanol, and deionized water, and was dried with  $\text{N}_2$ . In order to establish the sensing materials, ZnO nanowires were directly grown on the IDA by vapor-phase transport process. Note that the ZnO nanowires selectively grow on the lithographically structured Au layer of IDA while the density and thickness of the ZnO nanowires can be well controlled by fixed optimum growth conditions [9]. Briefly, a mixture of ZnO and graphite powders in a 1:1 ratio by weight was placed at the 950 °C position of the horizontal (vacuum tight ) two-zone the furnace as vapor source and the IDA at the 750 °C position as substrate. The NW synthesis was carried out at 30 mbar under a constant flow rate of 30 sccm Ar (99.9999%) and 1.5 sccm Ar/ $\text{O}_2$  mixture (Ar/ $\text{O}_2$  ration of 90/10, purity 99.999%) for 20 min. By vapor phase deposition, the ZnO NWs grew densely and perpendicular or slightly tilted on the electrodes. Hence, at the interdigitated pads, the ZnO NWs grow across the electrodes with many touching points air-bridged between the nanowires from adjacent contact pads forming a metal-semiconductor-semiconductor-metal device. The sensing of ZnO NWs results from resistance modulation of the ZnO NWs across two electrodes as shown in the schematic device in Fig. 1a. To further establish different sensing materials, the ZnO nanowires were coated homogeneously with 5 nm oxides

such as  $\text{Al}_2\text{O}_3$  and  $\text{TiO}_2$  by atomic layer deposition (ALD) to obtain core-shell nanostructures. The  $\text{Al}_2\text{O}_3$  and  $\text{TiO}_2$  were formed at 115 °C by reacting trimethylaluminum or titanium isopropoxide, respectively, with water vapor in a vertical flow type reactor (OpAL, Oxford Instruments). The coated samples were subsequently annealed at 700 °C for 3 h to achieve  $\text{ZnAl}_2\text{O}_4$  or  $\text{Zn}_2\text{TiO}_4$  on the surface of ZnO nanowires, respectively, based on solid-state reactions [10].

All three NWs gas sensors including the ZnO, ZnO- $\text{ZnAl}_2\text{O}_4$  core-shell, and ZnO- $\text{Zn}_2\text{TiO}_4$  core-shell NWs sensing parts were used to characterize toxic and non-toxic gases at room temperature. A UV LED ( $\lambda \sim 356$  nm and optical power  $\sim 200$   $\mu\text{W}$ ) was mounted above the sensors for photo-stimulation. These gas sensor array will be later integrated on the handling PCB for an E-nose. Before introducing gases into the measuring chamber, the chamber was evacuated down to  $\sim 10^{-3}$  mbar, followed by purging of synthesized air. This cycle was repeated several times. After that, different gases, such as  $\text{O}_3$ , CO and  $\text{NO}_2$  with a concentration between 100 ppb and 1 ppm and  $\text{O}_2$  with a concentration of 5% to 80% in nitrogen were individually led into the chamber adjusted by mass flow controller. During sensing, the UV LED was switched off in presence of target gases and was switched on when the target gas was removed. Theoretically, a large photocurrent will be induced by switching on/off the above-band-gap excitation due to photogenerated carriers [11]. The resistance minima in absence of target gas ( $R_0$ ) and maxima in target gas ( $R_G$ ) of the nanomaterials were recorded and the response of the sensor (S) is defined as ( $S = |(R_G - R_0)/R_0| \times 100\%$ ). Next, the sensor response data from all sensors were introduced into principal component analysis (PCA) to provide classification/qualification results of the sensors upon toxic and non-toxic gases. The PCA is a multivariate technique that

transforms the overall information into a set of new linear combinations of orthogonal variables called principal components (PC) without heavy loss of important original information.

### 3. Results and Discussion

The electrode was designed with a gap size between adjacent electrodes of 3  $\mu\text{m}$  as shown in the inset of Fig. 1b. After the growth of ZnO NWs, adjacent electrodes are electrically connected by cross ZnO NWs (Fig. 1c). The diameter and length of ZnO NWs were in the range of 60-180 nm and a few tens of  $\mu\text{m}$ , respectively. As one can see in the inset of Fig. 1c, the ZnO NWs are self-assembled between the gaps of electrodes. This electrical connection by a simple self-assembly process during synthesis reduces tedious and time consuming task comparing with other nanowire-based gas sensor fabrication techniques [12-14]. With the growth condition used here in our vapor phase deposition chamber, the density of ZnO NWs is also well-controlled. The nanowires are single-crystalline with the typical [0002] elongation (*c*-oriented) and follow the VS growth mechanism as shown in Fig. 2a.

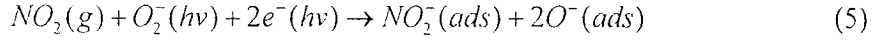
To investigate formation of ZnO-ZnAl<sub>2</sub>O<sub>4</sub> core-shell and ZnO-Zn<sub>2</sub>TiO<sub>4</sub> core-shell nanowires, Fig. 2b and 2c presents the TEM images of structures after annealing ZnO-Al<sub>2</sub>O<sub>3</sub> and ZnO-TiO<sub>2</sub> nanowires under identical conditions. For ZnO-ZnAl<sub>2</sub>O<sub>4</sub> core-shell nanowires, cavities distributed along the interface clearly show the existence of bridge-like linkages between the residual ZnO core and the spinel ZnAl<sub>2</sub>O<sub>4</sub> shell (see Fig. 2b) after solid-solid reaction. The one-way interfacial bulk diffusion of ZnO into the amorphous Al<sub>2</sub>O<sub>3</sub> shell can form the ZnAl<sub>2</sub>O<sub>4</sub> at shell and generate a series of cavities at the interface due to the Kirkendall effect [10]. Unlike the reaction of ZnO-Al<sub>2</sub>O<sub>3</sub> nanowires, no cavity was observed at ZnO-Zn<sub>2</sub>TiO<sub>4</sub> core-shell interface (see Fig. 2c), indicating the interdiffusion between ZnO and TiO<sub>2</sub> was not dominated by

the Kirkendall effect in this case. Apparently, from the electron diffraction patterns, the unreacted ZnO NWs cores still keep the single-crystal nature while the formed  $\text{ZnAl}_2\text{O}_4$  and  $\text{Zn}_2\text{TiO}_4$  are polycrystalline with a rough surface feature.

It is well known that the gas sensitivity of ZnO NWs comes from the trapping of the gas molecules on the surface which can modulate the surface depletion layer width [15]. The negative charges at the surface of n-type semiconductor usually generate an upward electronic band-bending along the diameter of ZnO NWs [16]. The surface charges influence the surface-band potential and cause a stronger or a weaker band-bending. This modulation of band-bending directly makes a change in the conduction of ZnO NWs. Figure 3a demonstrates the dynamic responses of nanowires sensors to oxidizing  $\text{NO}_2$  gas at room temperature under UV illumination. The electrical resistance of all the sensors increases at the moment of  $\text{NO}_2$  exposure. By applying UV illumination during the gas sensing process, electron-hole pairs are generated in sensing materials. The photo-generated holes can migrate to the surface via the electric field induced by the band bending and react with adsorbed oxygen species ( $\text{O}_2^-(\text{ads})$ ). At the same time, the photo-generated electrons react with additional photoinduced oxygen ions, resulting to form photostimulated oxygen species ( $\text{O}_2^-(\text{ads})$ ) at the shell surfaces as the following schemes [17]:



Upon exposure to  $\text{NO}_2$ ,  $\text{NO}_2$  molecules come to react with the photostimulated oxygen species on the surface to capture available free electrons in the following reaction:



This reaction increases the concentration of holes that enlarged the band bending, leading to an increase of depletion layer width. Therefore, resistance of core-shell nanowire sensor increases with increasing  $NO_2$  concentration. Moreover,  $NO_2$  can also directly capture the electrons from the conduction band due to its higher electrophilic properties [18].

From Fig. 3b, at low  $NO_2$  concentrations (100-300 ppb), the  $ZnO-Zn_2TiO_4$  core-shell nanowire sensor shows high response to  $NO_2$  over other sensors (more than 50%) due to more surface roughness for specific  $NO_2$  adsorptions while it also shows medium sensitivity to  $O_2$  and relatively low sensitivity to  $CO$  and  $O_3$ . For the  $ZnO$  nanowire sensor, it is sensitive to most of gasses. The cross-sensitivity problem makes its selectivity of  $ZnO$  nanowire to be low. This may provide an ambiguous response in terms of individual components of the gas mixtures. In case of  $ZnO-ZnAl_2O_4$  core-shell nanowires, it exhibits high sensitivity and selectivity to  $NO_2$ . This refers to the good performance for  $NO_2$  detection in real world application. The  $NO_x$  species prefer to adsorb on the  $ZnAl_2O_4$  surface over other gases via  $\pi^*(N)$  transitions [19]. Enhancement of sensing properties of core-shell nanowires over  $ZnO$  nanowires may result from the contribution of n-n heterojunction that can adjust energy barrier height and modulate electron transport [20]. In comparison between  $ZnO-Zn_2TiO_4$  and  $ZnO-ZnAl_2O_4$  core-shell nanowires, the different sensing properties cause from different rough surface feature and intrinsic material properties. The rough surface feature of the  $ZnO-Zn_2TiO_4$  improves the efficiency and the amount of oxygen chemisorptions [21] resulting in an enhancement of gas responses on all target gases over the  $ZnO-ZnAl_2O_4$ . The  $Al_{Zn}$  antisite defects in  $ZnAl_2O_4$  spinel were found to act as a shallow donor and Al-O bond appears more ionic [22]. This can contribute to charge transports between

$\text{NO}_2$  and  $\text{ZnO-ZnAl}_2\text{O}_4$  core-shell nanowires leading to higher selectivity of the  $\text{ZnO-ZnAl}_2\text{O}_4$  core-shell towards  $\text{NO}_2$ .

To evaluate the discrimination power of core-shell sensor array, the PCA was carried out with the relative response feature extraction technique [2]. As shown in Fig. 4, the PCA result is clearly separated to 4 clusters corresponding to the 4 different target gases. No overlap between different gas species occurs in PCA. It indicates the high performance of such nanowire gas sensor array for detection and discrimination of both oxidizing and reducing gases at room temperature over other pervious work that usually operated at high temperatures ( $>200\text{ }^\circ\text{C}$ ) [7, 23]. Here we demonstrate that the NW e-nose based on ZnO NWs and surface modification can be used to identify both gas type and the concentration of gases at room temperature. The ZnO NW e-nose which can operate at room temperature will be very useful in term of energy conservation.

#### 4. Conclusion

In summary, we propose a simple but reliable method for the ZnO NW E-nose fabrication. The E-nose composed of three nanowire sensors which are ZnO nanowires,  $\text{ZnO-ZnAl}_2\text{O}_4$  core-shell nanowires, and  $\text{Zn}_2\text{TiO}_4$  core-shell nanowires. The photolithography was used to pattern and identify the ZnO NWs structure. The ZnO NWs were grown by vapor phase deposition and the result from the growth is the cross nanostructure of ZnO NWs between two electrodes. The sensor was then deposited by ALD before annealing process. After an annealing at  $700\text{ }^\circ\text{C}$ , the solid reactions were completed. All three sensors were used to sense  $\text{NO}_2$ , CO,  $\text{O}_2$ ,  $\text{O}_3$  at room temperature. Based on photostimulation by UV, oxygen species ( $\text{O}_2^-$ ) can be generated to adsorb on the nanowire surface for interacting with gas molecules. The

results shows that ZnO nanowire cannot use as a potential single gas sensor for detection of toxic gas in envelopment at room temperature due to cross sensitive problem of ZnO surface while  $\text{ZnAl}_2\text{O}_4$  surface shows high sensitivity and selectivity to  $\text{NO}_2$  and  $\text{Zn}_2\text{TiO}_4$  exhibits improvement of gas response of toxic gas ( $\text{NO}_2$  and CO) at low concentration (100-300 ppb) due to high surface area. By combined three nanowire sensor, the microelectronic nose has great potential to detect and discriminate a wide variety of gases including toxic gases and non-toxic gases.

### Acknowledgments

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## Lists of Figures

**Figure 1:** a) Schematic structure of gas sensor for an E-nose. SEM images of b) finger grid interdigitated electrode and c) ZnO NWs grown on the IDA.

**Figure 2:** TEM images and their corresponding ED patterns of (a) ZnO nanowire, (b) ZnO-ZnAl<sub>2</sub>O<sub>4</sub> core-shell nanowire, and (c) ZnO-Zn<sub>2</sub>TiO<sub>4</sub> core-shell nanowire.

**Figure 3:** (a) Real time NO<sub>2</sub> detection and (b) responses to various NO<sub>2</sub>, CO, O<sub>2</sub>, O<sub>3</sub> concentrations of ZnO nanowires, ZnO-ZnAl<sub>2</sub>O<sub>4</sub> core-shell nanowires, Zn<sub>2</sub>TiO<sub>4</sub> core-shell nanowires at room temperature.

**Figure 4:** 3D principal component analysis plot of three nanowire gas sensors for discriminating a variety of gases at room temperature.

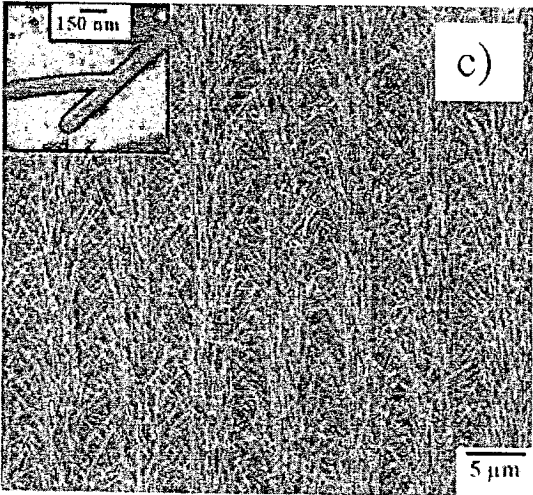
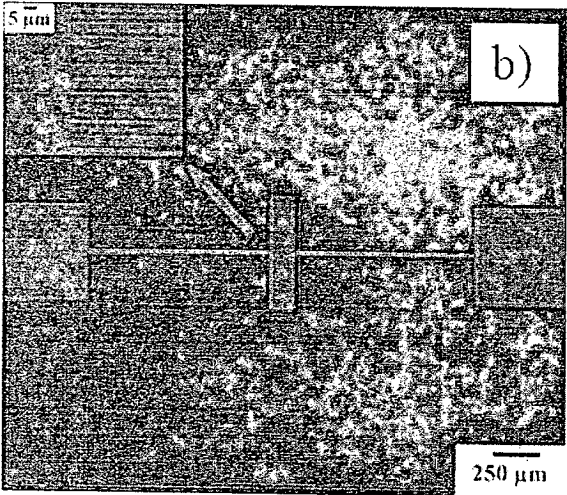
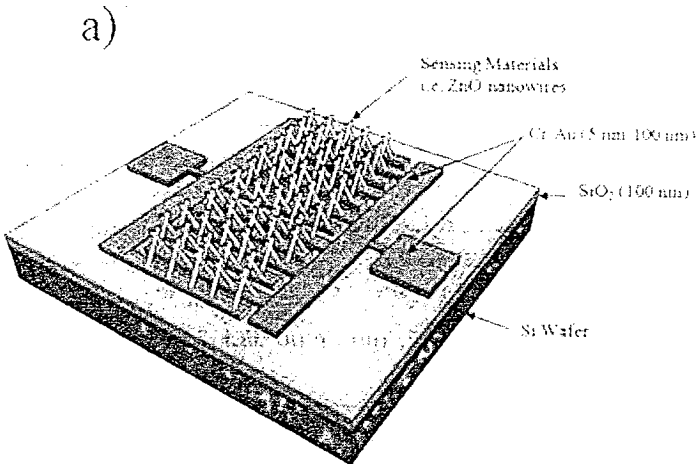


Figure 1

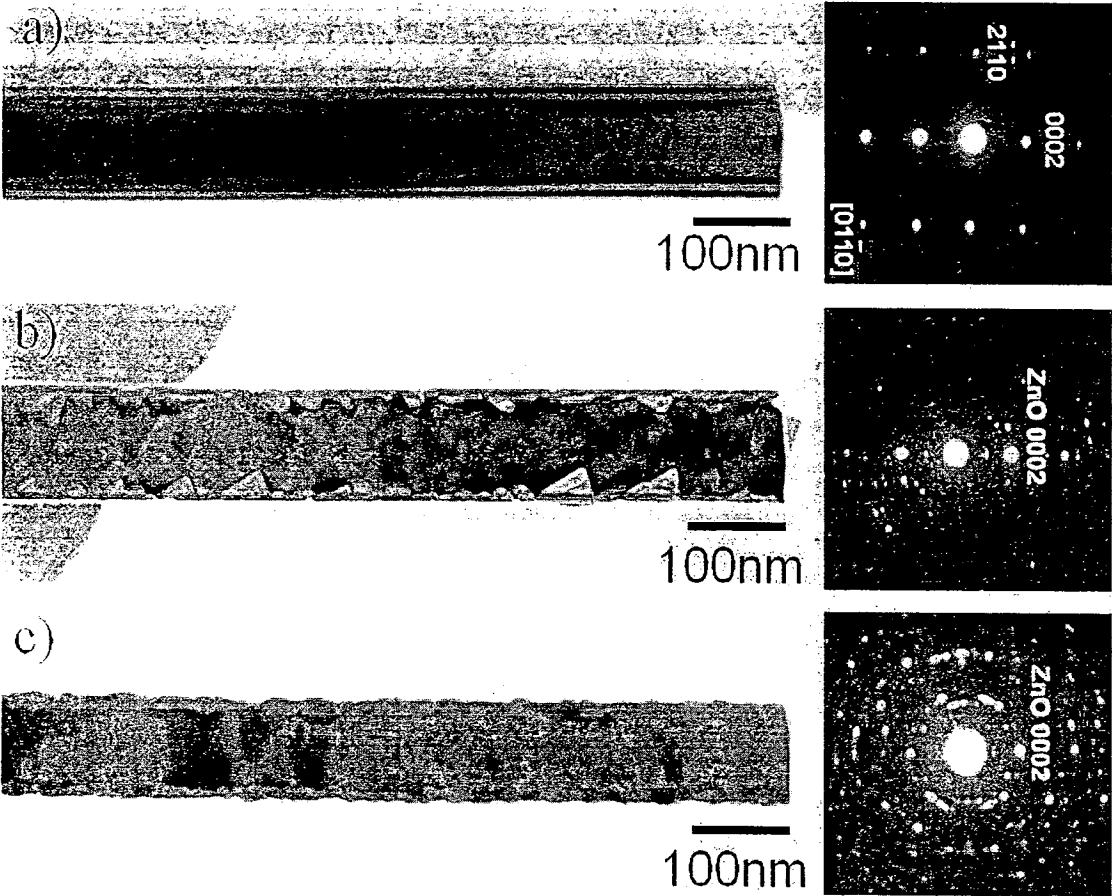


Figure 2

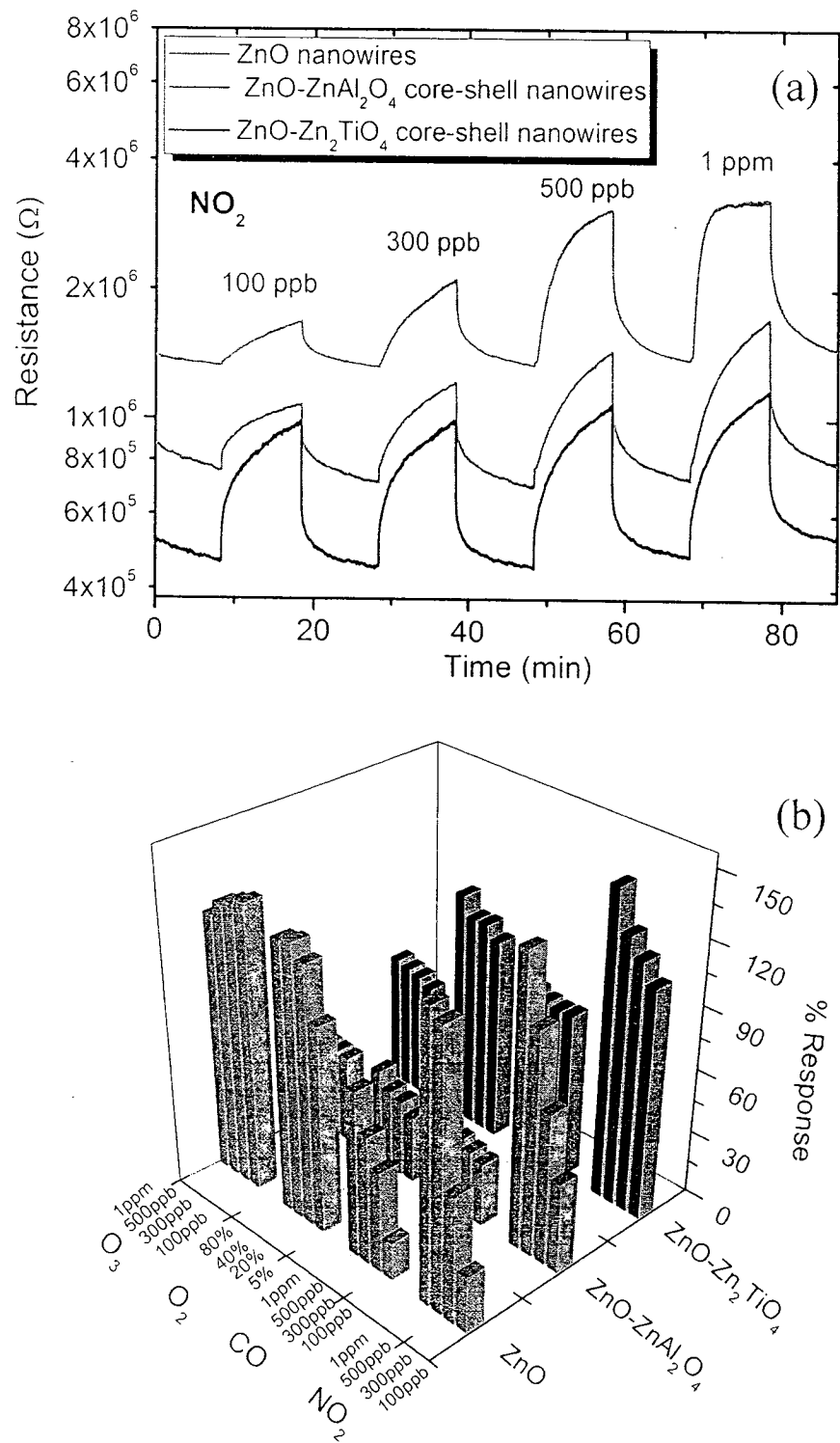


Figure 3

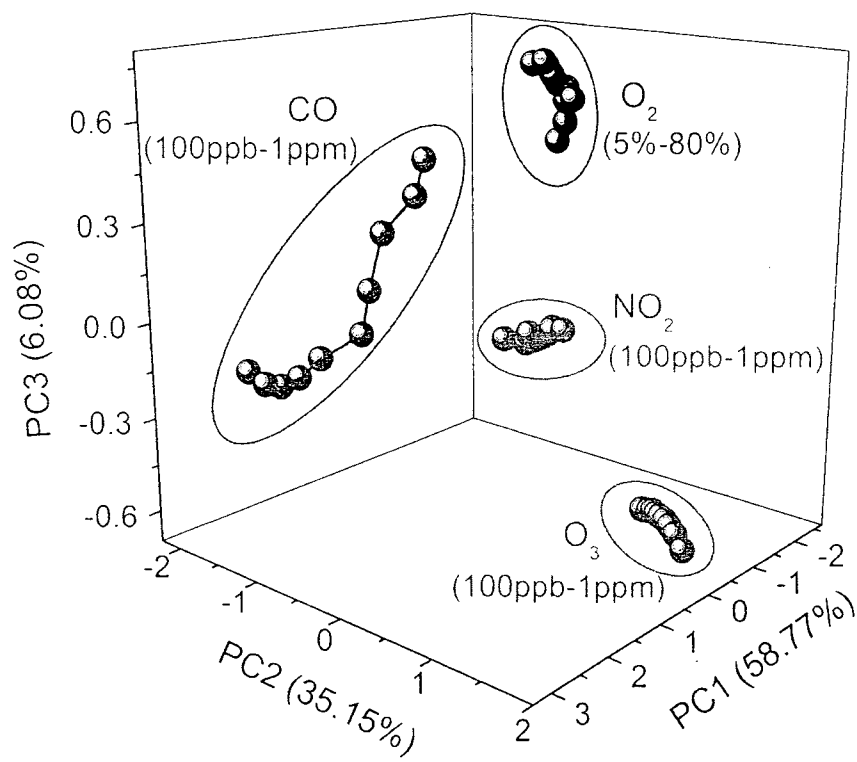


Figure 4

# Development of Networked Electronic Nose Based on Multi-walled Carbon Nanotubes/Polymer Composite Gas Sensor Array

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## Abstract

In this paper, we have presented the design and invention of an electronic nose (E-nose) that can work and analyze the results via a network system such as LAN or WiFi. The MWCNTs/polymer composites were used as a gas sensor array. The constant current circuit was newly designed for gas sensor measurement. The fabricated E-nose showed a high performance for indoor air monitoring with very low noise.

**Keywords:** E-nose, polymer sensor, indoor air monitoring, E-nose circuits, PS/CNT sensor, gas sensor array

## Introduction

Recent decades have observed significantly increasing interest in the applications of electronic nose (E-nose) ranging from quality control of foods [1,2] and beverages [3,4], environment protection [5], medical applications [6] to human identification [7,8]. Because E-nose offers many advantages in the analysis of volatiles, i.e. a low detection limit, cost- and time effectiveness, robustness, simplicity, and operator independence [9]. In principles, an E-nose consists of three main parts: (i) air flow system, (ii) detection system, and (iii) control and data analysis system [10]. For air flow system there are two main types of flow systems including static and dynamic flow systems. In detection system, sensor array with measurement circuit is used to detect the aroma molecules. For data analysis system, pattern recognition and machine learning such as artificial neural networks (ANN), linear discriminant analysis (LDA), support vector machine (SVM), and principal components analysis (PCA) are typically used in data analysis on a computer. Although E-nose has been in the market for several years, development of E-nose is still necessary to provide opportunities for new applications.

In this work, we have presented the development of an E-nose that can work and analyze the results via a network system such as LAN and WiFi. The fabrication of room temperature gas sensor array will be proposed. The measurement circuits of the networked E-nose will be highlighted. The constructed networked E-nose will also be demonstrated for uses in real world applications such as indoor air monitoring.

## Experimental Details

### A. Treatment of Carbon Nanotubes

Multi-walled carbon nanotubes (MWCNTs) were dispersed in a solution of ethanol and NaOH/ethanol using ultrasonication for 30 min. The NaOH/ethanol solution contained 150 g/l of NaOH in 80 vol% ethanol and 20 vol% water. The dispersion was filtered by using a syringe micro-filter system with a nylon micro-filter and then washed with ethanol until the pH value of the filtrate was about 7. After this treatment, the remaining filtered and dried MWNTs can be easily dispersed in different solvents.

### B. Preparation of MWCNTs/Polymer Composite Sensor array

The sensor elements consist of interdigitated gold electrodes deposited on aluminum oxide substrate (2x2.5 mm). In order to prepare MWCNTs/polymer composite, polystyrene (PS) and polystyrene-co-maleic acid (PS-Maleic AC) were employed as the polymer matrices while dimethylformamide (DMF) and tetrahydrofuran (THF) were used as solvents. Four different conditions of CNTs/polymer composites were produced as summarized in Table I. The deposition of the CNTs/polymer composites on the sensor element was achieved by drop coating using a micro pipette, Gilson Pipetman P20.

TABLE I  
DEPOSITION CONDITIONS FOR THE MWCNTS/POLYMER COMPOSITE COATING

Sensor Number	Polymer / MWCNT	Solvent	Drop amount	Substrate Temp
1	PS	THF	5 $\mu$ l	80 $^{\circ}$ C
2	PS	THF	3 $\mu$ l	80 $^{\circ}$ C
3	PS-Maleic Ac	THF	3 $\mu$ l	25 $^{\circ}$ C
4	PS	DMF	3 $\mu$ l	80 $^{\circ}$ C

### C. Fabrication of Networked E-nose

The networked E-nose consists of three main parts including

(i) air flow system, (ii) detection system, and (iii) control and data analysis system. The air flow system refers to the way to deliver aroma molecules into the detection system. In this networked E-nose, a simple dynamic flow system was employed. The gas sensor array was installed at the bottom of the rectangular chamber. The air carrying the odor molecules can be introduced into the sensor chamber through a hole with an area of  $4\text{ cm}^2$ . In the detection system, a constant current circuit as shown in Fig. 1 was used to measure the resistance of the gas sensor array. The constant current measurement circuit consists of an operational amplifier in a constant current configuration of  $500\text{ }\mu\text{A}$  with the sensor array to be measured in the feedback loop (see Fig. 1a). Each side of the sensor was connected to a discrete buffer circuit consisting of an operational amplifier in the voltage follower configuration as shown in Fig. 1b. The buffer circuit separates the constant current circuit from the differential amplifier to prevent a disturbance of the current source. The differential amplifier calculates the difference between the two input voltages and multiplies the result by a gain factor. If  $R_3=R_4$  and  $R_2=R_5$ , the gain factor was  $R_2/R_3$ . In Fig. 1c,  $R_3$  and  $R_4$  were  $1\text{ k}\Omega$  while  $R_2$  and  $R_5$  were  $2\text{ k}\Omega$ , so the gain factor was 2. For example, if the resistance of the sensor was  $1\text{ k}\Omega$ , the current of  $500\text{ }\mu\text{A}$  produced a voltage difference of  $0.5\text{ V}$ . Therefore, this voltage difference of  $0.5\text{ V}$  was amplified by a factor of 2, so the resulting output voltage was  $1\text{ V}$ .

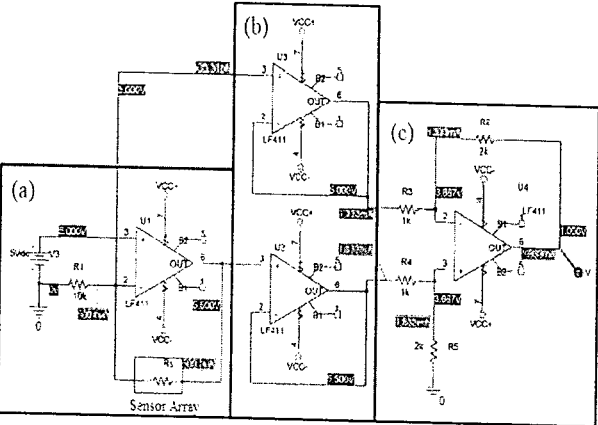


Fig. 1 Measurement circuit with an output of 0-10 V (1 mV/ $\Omega$ ) including (a)  $500\text{ }\mu\text{A}$  constant current source, (b) buffer circuit and (c) differential amplifier having gain of 2.

Instead of using a single sensor, an analog multiplexer can be used to select one out of many sensors to be measured as shown in Fig. 2. In such a case, each sensor was connected to one input of the analog 8-channel multiplexer. The multiplexer internally connected only one input to its output. The input-to-output connection was selected by a digital input.

In the control and data analysis system, microchip PIC24FJ48GA002 microcontroller was used to control the measurement systems. The CS5526 was used as the A/D converter. The measurement software was written by LabVIEW. The data from networked E-nose was stored and transferred into a Laptop every second via a small WiFi-Router for subsequent analysis.

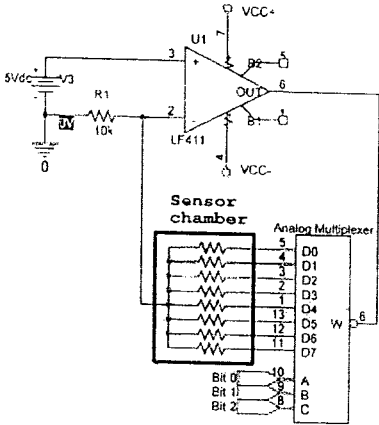


Fig. 2 Connection of gas sensor array with 8-channel multiplexer circuit.

### Results and Discussion

#### A. Electronic Circuit Test

As the design measurement circuits, the sampling rate can be programmed ranging from 3.76 samples per second up to 202 samples per second. Note that the noise level and resolution depends on the sampling frequency.

TABLE II  
RMS NOISE OF DESIGN MEASUREMENT CIRCUIT

Output Rate (Hz)	-3 dB Filter Frequency	Input Range (Bipolar/Unipolar Mode)					
		25 mV	55 mV	100 mV	1 V	2.5 V	5 V
3.76	3.27	90 nV	90 nV	130 nV	1 $\mu\text{V}$	2 $\mu\text{V}$	4 $\mu\text{V}$
7.51	6.55	110 nV	130 nV	190 nV	1.5 $\mu\text{V}$	3 $\mu\text{V}$	7 $\mu\text{V}$
15.0	12.7	170 nV	200 nV	250 nV	2 $\mu\text{V}$	5 $\mu\text{V}$	10 $\mu\text{V}$
30.1	25.4	250 nV	300 nV	500 nV	4 $\mu\text{V}$	10 $\mu\text{V}$	15 $\mu\text{V}$
60.0	50.4	500 nV	1 $\mu\text{V}$	1.5 $\mu\text{V}$	15 $\mu\text{V}$	45 $\mu\text{V}$	85 $\mu\text{V}$
123.2	103.6	2 $\mu\text{V}$	4 $\mu\text{V}$	8 $\mu\text{V}$	72 $\mu\text{V}$	190 $\mu\text{V}$	350 $\mu\text{V}$
168.9	141.3	10 $\mu\text{V}$	20 $\mu\text{V}$	30 $\mu\text{V}$	340 $\mu\text{V}$	900 $\mu\text{V}$	2 mV
202.3	169.2	30 $\mu\text{V}$	55 $\mu\text{V}$	105 $\mu\text{V}$	1.1 mV	2.4 mV	5.3 mV

TABLE III  
RESISTANCE RESOLUTION OF MEASUREMENT CIRCUIT

Output Rate (Hz)	Resistance Range					
	2.5 k $\Omega$	5.5 k $\Omega$	10 k $\Omega$	100 k $\Omega$	250 k $\Omega$	500 k $\Omega$
3.76	0.06 $\Omega$	0.06 $\Omega$	0.09 $\Omega$	0.66 $\Omega$	1.32 $\Omega$	2.64 $\Omega$
7.51	0.07 $\Omega$	0.09 $\Omega$	0.13 $\Omega$	0.99 $\Omega$	1.98 $\Omega$	4.62 $\Omega$
15.0	0.11 $\Omega$	0.13 $\Omega$	0.17 $\Omega$	1.32 $\Omega$	3.3 $\Omega$	6.6 $\Omega$
30.1	0.17 $\Omega$	0.2 $\Omega$	0.33 $\Omega$	2.64 $\Omega$	6.6 $\Omega$	9.9 $\Omega$
60.0	0.33 $\Omega$	0.66 $\Omega$	0.99 $\Omega$	9.9 $\Omega$	29.7 $\Omega$	56.1 $\Omega$
123.2	1.32 $\Omega$	2.64 $\Omega$	5.28 $\Omega$	47.52 $\Omega$	125.4 $\Omega$	231 $\Omega$
168.9	6.6 $\Omega$	13.2 $\Omega$	19.8 $\Omega$	224.4 $\Omega$	594 $\Omega$	1320 $\Omega$
202.3	19.8 $\Omega$	36.3 $\Omega$	69.3 $\Omega$	726 $\Omega$	1584 $\Omega$	3498 $\Omega$

Table II shows the dependence of voltage noise by the sampling rate while Table III shows the resistance resolution for  $10\text{ }\mu\text{A}$  constant current depending on the sampling rate. To



calculate the resistance resolution, the peak-to-peak noise voltage was calculated first by multiplying the RMS noise voltage by 6.6 and then divided by 10  $\mu$ A.

The best ratio of performance and speed of measurement was achieved by using 15 Hz sampling rate. From the Tables, at an input range of 25 mV and 15 Hz sampling rate, the peak-to-peak noise of the resistance, using 10  $\mu$ A constant current, was only about 0.11  $\Omega$ . This design circuit with low noise can also support the measurement of resistance from many gas sensor elements up to 64 gas sensors.

### B. MWCNTs/Polymer Composite Characterization

The pure dispersed MWCNTs and MWCNTs/polymer composites were investigated by using a scanning electron microscope (SEM) as displayed in Fig. 3 and 3b, respectively. Using chemical treatment, the MWCNTs were quite well dispersed in solvents (see Fig. 3a). The diameters of MWCNTs are within a range of 60-180 nm. After the deposition of the MWCNTs/polymer composites on the sensor element, SEM image (see Fig. 3b) showed the insertion of MWCNTs inside the hole of polymer. Creation of these nanochannels can be expected to enhance the surface-to-volume ratio and reactivity between gas molecule and sensing material [11,12] leading to an increase in the sensitivity of typical polymer gas sensor.

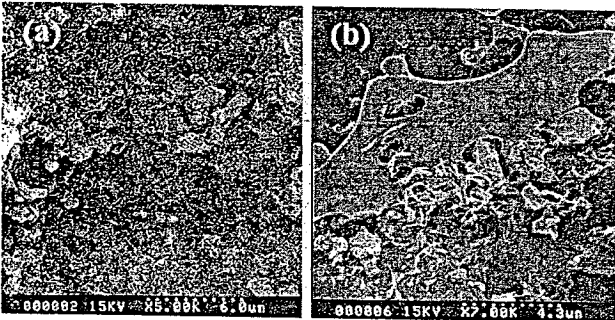


Fig. 3 SEM images of (a) pure dispersed MWCNTs and (b) MWCNTs/PS composite surfaces.

### C. Indoor Air Monitoring

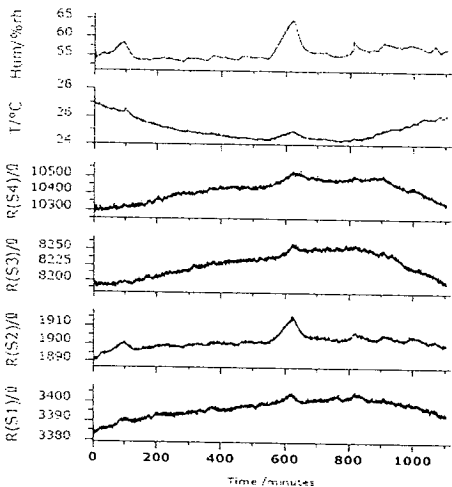


Fig. 4 Gas sensor signals from long time measurement in a room.

The sensor elements showed a highly selective sensitivity to acetic acid vapors but as good as no response to ethanol, methanol and water vapor. The long-term stability of the sensor elements was tested over a period of 18.5 hours in normal air in the laboratory. It can prove that this networked E-Nose based on MWCNTs/polymer composite gas sensor array can be used to monitor the environment with low noise (See Fig. 4).

### Conclusion

The design and implementation of a networked E-nose has been presented for online detection of indoor air. The MWCNTs/polymer composite gas sensors as prepared by drop coating technique were used as a gas sensing array. The new designed constant current circuit was employed to measure the resistance of gas sensor array. The results showed the designed measurement circuit with very low noise (at sampling rate < 100 Hz, the relative noise < 0.02% ) and insertion of MWCNTs inside the hole of polymer that can enhance the sensitivity of typical polymer gas sensor. It is hoped that this work will have many uses for new development of low cost networked E-nose system for indoor air monitoring.

### Acknowledgments

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# Diabetes Diagnosis by Direct Measurement from Urine Odor Using Electronic Nose

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**Abstract**—Diabetes is one of the most common chronic diseases and can occur at any age. To avoid many side effects of diabetes on health, early detection of diabetes is very necessary. In this paper, we propose an alternative method to detect diabetes based on direct measurement of urine odor by using an electronic nose (E-nose). Artificial urines, used to simulated a situation of diabetes patient, were produced by adding glucose into the pure urine samples. Eight commercial chemical gas sensors were used as the sensing elements of our e-nose. Principal components analysis (PCA) and cluster analysis (CA) methods were employed for data analysis. The PCA and CA results show that the proposed method was able to identify the glucose concentration in urine. In the future, e-nose can be a potential tool for diabetes diagnosis for healthcare personnel as well as home users.

**Index Terms**—E-nose, PCA, smart toilet, chemical sensor, diabetes.

## 1. INTRODUCTION

Diabetes is one of the most common chronic diseases caused by metabolic malfunction in carbohydrate metabolism. In the report of World Health Organization (WHO) based on August 2011, there are 364 million diabetes patients in the world and more than 80% of diabetes deaths occur in low-and middle-income countries. In Thailand, the Bureau of Noncommunicable Disease reported that there were about 0.6 million diabetes patients in 2010. The data shows that diabetes is an important disease that can occur in every people. Diabetes occurs either when the pancreas does not produce enough insulin or when the body cannot effectively use the insulin it produces. Insulin is a hormone that regulates blood glucose levels. Hyperglycaemia is a common effect of uncontrolled diabetes and over time leads to serious damage to many of the body's system, especially the nerves and blood vessels. The diabetes diagnosis can be made by measurement of glucose level in blood. In general, there are three methods including; (i) fasting plasma glucose test, (ii) oral glucose tolerance test, and (iii) random plasma glucose test for diabetes

diagnosis. All of these methods can measure the level of glucose but their procedures are quite complicated and time-consuming. Another method for fast diabetes diagnosis is the measurement of glucose in urine by using urine reagent strips. This method is quick and convenient but suffers low accuracy.

Electronic nose (E-nose) technology has been widely used in food industry, agriculture, environment monitoring and medical applications [1-5]. For example, the E-nose system was used to detect and discriminate exhaled breath of hepatocellular carcinoma patients [6] and diagnosis of urinary tract infection. [7].

In this paper, we have studied the possibility for diabetes diagnosis by direct measurement of urine odor using a lab-made e-nose. In general, urine contains very little glucose and other composition as shown in Table I. People with abnormal high blood sugar often have glucose in their urine because of diabetes. The effect of high level sugar in urine can cause a sweet or fruity odor. Therefore, e-nose may be applied for diabetes diagnosis of the urine odor directly.

TABLE I. COMPOSITION OF NORMAL URINE

Item	Amount (%wt)
Water	95
Inorganic salt	1.91
Urea	1.81
Organic ammonium salt	0.70
Organic compounds	0.56
Glucose	0.02

a. Data from "Nasa Contractor Report" [8]

II. EXPERIMENTAL DETAILS

Sample collection and Preparation

Urine samples were collected from normal people that ve normal level of glucose in urine. The samples were llected and measured the temperature and volume mediately. Next, the sample was tested with urine reagent ip to ensure the normal glucose level in urine. Various ncentrations of glucose (Glucolin, 99% of glucose) were ded into the pure urine samples in order to simulate the ificial urines of diabetes patients. Six different samples were duced as summarized in Table II.

TABLE II. THE DEFINITION OF EACH SPECIMEN

Definition	Item
Sample 1	Pure Urine
Sample 2	Pure Urine + 100 mg/dl glucose
Sample 3	Pure Urine + 250 mg/dl glucose
Sample 4	Pure Urine + 500 mg/dl glucose
Sample 5	Pure Urine + 1000 mg/dl glucose
Sample 6	Pure Urine + 2000 mg/dl glucose

Urine reagent strips testing

The urine samples were tested by urine reagent strips for imating the concentration of glucose. Urine strip was npletely dipped into the sample and immediately removed avoid dissolving of the reagent areas, waiting for 30 onds. The color change of the reagent area was compared he corresponding color chart on the bottle label.

Measurement by the Electric Nose

After testing the sample with urine reagent strips, the ples were measured by an E-nose. The schematic diagram our lab-made e-nose system was shown in Fig. 1. The perature of the sample was controlled by thermostat and ied as follows: 35, 40, and 45°C.

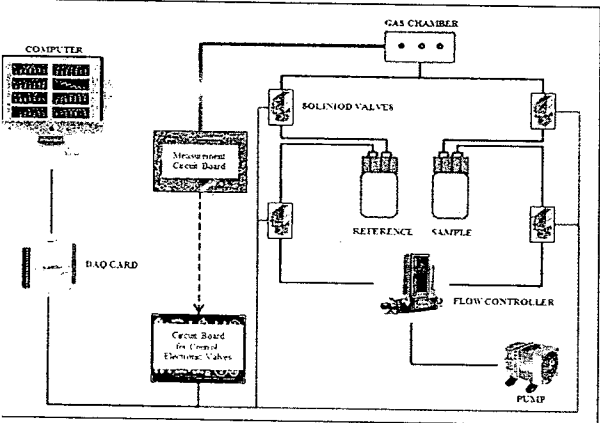


Fig. 1. The schematic diagram of E-nose system

III. RESULT AND DISCUSSION

A. Urine reagent strips testing

Based on adding of the amount of glucoses as summarized in Table II, the result of urine reagent strips testing is displayed in Fig. 2. The color of reagent area is in good agreement with the color chart of standard database. It indicates that artificial urine for diabetes patient can be simply produced by direct adding of glucose amounts summarized in Table II.

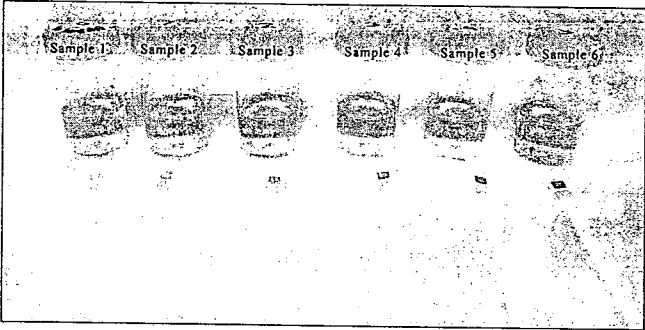


Fig. 2. Result of urine strip reagent testing

B. Sensor Response

The response of gas sensor ( $S_i$ ) was calculated by the following equation;

$$S_i = |R_0 - R_s| / R_0 \tag{1}$$

Where

$R_0$  is resistance of sensor in pure air  
and  $R_s$  is resistance of sensor in sample odors

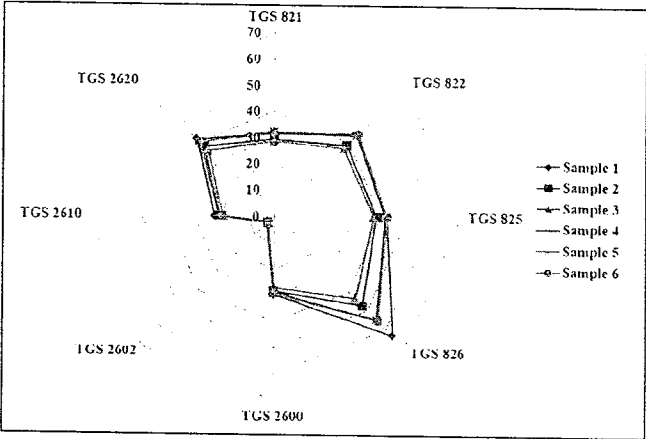


Fig. 3. Average sensor response of each sensor

The average sensor response was calculated and plotted against with the concentrations of glucose as shown in Fig. 3. The highest response of 65% is obtained from TGS 826 sensor while TGS 2602 sensor gives the lowest sensor response of 3% on sample 1.

From the datasheets of gas sensor (<http://www.figaro-sensor.com>), TGS 826 is the sensor for ammonia detection. From the composition of urine as show in Table I, there is

7 wt% of organic ammonia salt in urine so this causes the gh sensor response of TGS 826. In case of TGS 2602, this nsor is generally used for detection of air contaminants such toluene and hydrogen sulfide. Such contaminants are not ajor composition of urine. Therefore, the TGS 2602 sensor ows the lowest sensor response. However, the TGS gas nsors were not designed to detect the fruity odor. The sensor sponses are not linear with the glucose concentration but ey can generate the unique patterns. Therefore, the data will introduced into principal components analysis (PCA) and ister analysis (CA) for further data analysis.

### Principal Components Analysis (PCA)

To specify the level of glucose in urine, the principal nponents analysis (PCA) was used for pattern recognition. ine samples were measured by varying temperatures (35, 40, d 45°C). In principles, the increase of temperature has an ect to the evaporation rate of the solution that can cause tinct sensor response.

At temperature of 35°C, the result of PCA is not clearly arated in each concentration as shown in Figure 4 (a). When temperature increases to 40°C, there is a bit shift of sample 1 m other samples. Almost all samples are still grouped within same region. For the temperature at 45°C, the PCA result arly shows the separation of normal urine from other nples. There are two groups that can be noticed as shown in . 4 (c). The left side is low concentration of glucose and ht side is moderate and high concentrations of glucose.

### Cluster Analysis (CA)

To study the distinction of PCA point in each experiment, cluster analysis method (CA) was used. The results are own in Fig. 5. At the temperature of 35°C and 40°C, the CA ults scatter conformably to the PCA results. These peratures cannot identify the normal people that have mal level of glucose in urine. High order of CA result was erved when the temperature of measurement increases to C. There is two large groups. First group is sample 1 and pple 2. Second group is sample 3, 4, 5 and 6. For first group, e is a little similarity of PCA point. The result conforms to PCA results as shown in Fig 4 (c). For the second group, pple 5 can be clearly separated from the samples 3, 4 and 6. m cluster analysis, it can be concluded that the increase of perature during measurement can increase the possibility of tronic nose for diabetes diagnosis.

### IV. CONCLUSION

The study of diabetes diagnosis by direct measurement n urine odor with electronic nose was achieved with /ing the temperatures. The commercial TGS gas sensors e used as the sensing section and the highest sensitivity was erved from TGS 826 sensor that can detect gas ammonia. PCA and CA method were employed in data analysis.

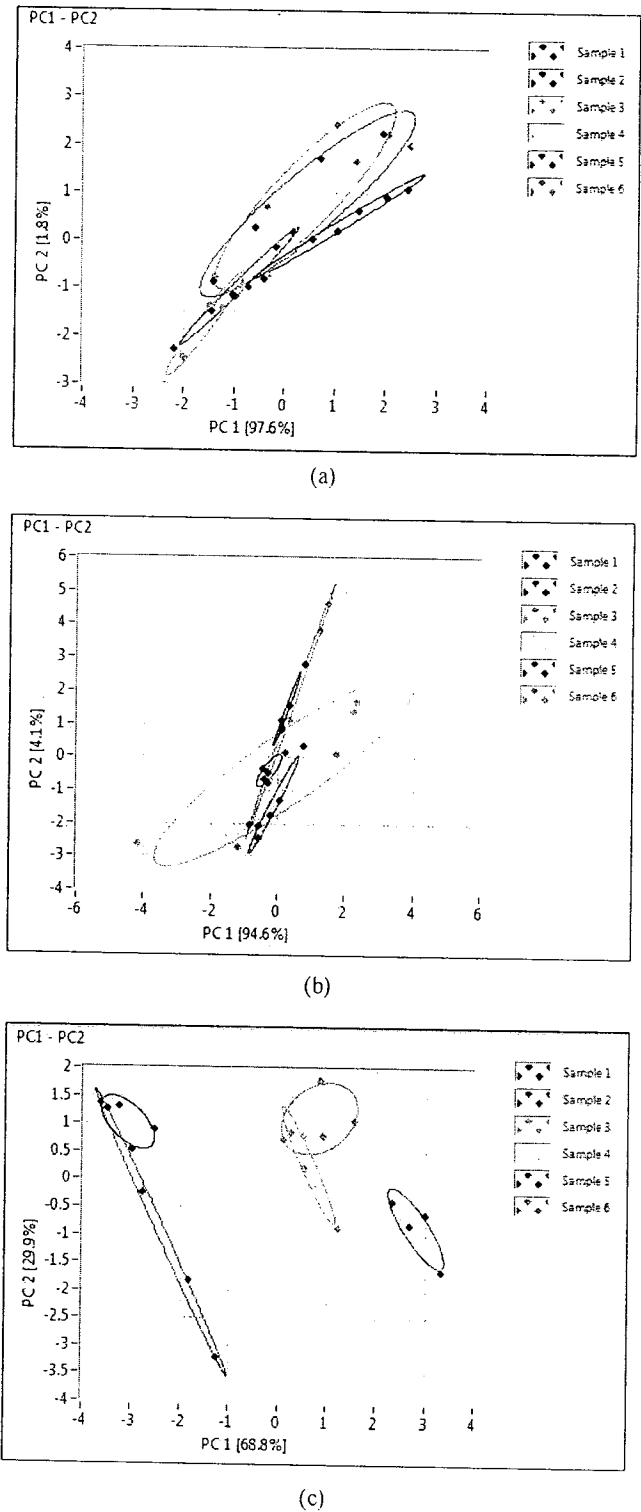
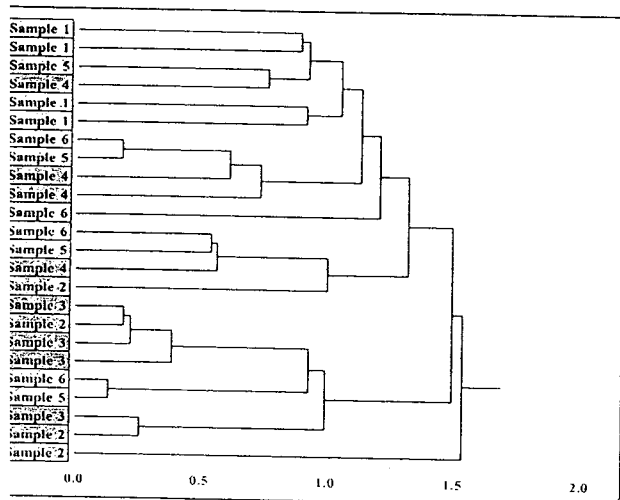
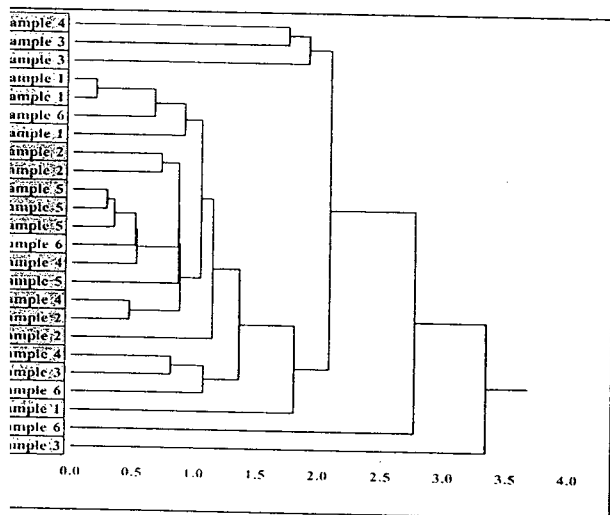


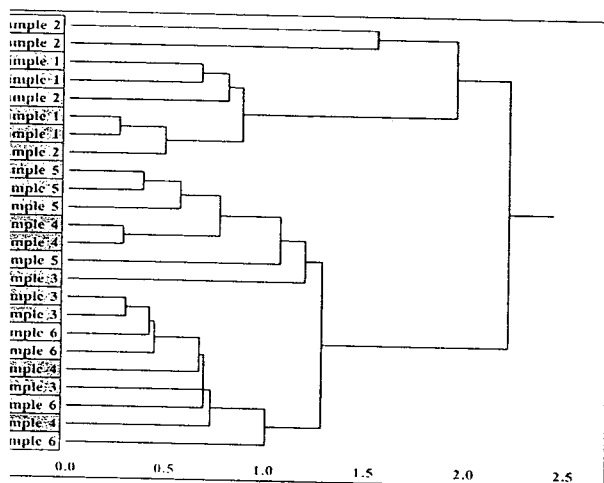
Fig. 4. Principal Components Analysis (PCA) of glucose in urine as various temperature (a) 35°C, (b) 40°C, and (c) 45°C



(a)



(b)



(c)

5. Cluster Analysis (CA) of glucose in urine as various temperatures (a) 35°C, (b) 40°C, and (c) 45°C

From the PCA and CA results, it was shown that the increment of sample temperature can increase the possibility for identification of the concentration of glucose in urine. Based on this preliminary study, our lab-made e-nose can be a potential device for diabetes diagnosis by direct measurement from urine odor with applied the temperature ( $>45^{\circ}\text{C}$ ).

## ACKNOWLEDGMENT

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## Bread Baking Aroma Analysis by an Intelligent Electronic Nose System for Future Robotic Chef

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### Abstract

Electronic nose (E-nose) is an instrument that can be used to detect and distinguish volatile organic compounds (VOCs) with high accuracy and fast operating time. The E-nose can be applied to various fields such as food analysis, medicine, environmental control, and industrial processes. Combined with robot technologies (robotic chef), the E-nose may be installed and used to detect food aromas during cooking process. In this work, we have developed the E-nose for robotic chef noses. An example of application for robotic chef noses has been demonstrated in case of bread baking aromas detection. The bread baking process has been varied at four different baking temperatures of 40, 60, 80, and 100 °C and four different baking time of 5, 10, 15, and 20 minutes. The percentage changes of sensor resistance and principal component analysis (PCA) method have been employed to analyze the data. The results show that the E-nose can detect bread baking aromas and clearly classify the bread with baking process at different conditions. This study will be useful for robotic chef noses in various food quality applications in near future.

**Keywords:** E-nose, food quality control, PCA method, robotic chef

### Introduction

Electronic nose (E-nose) is an olfactory sensing system that mimics mammalian nose for detection of volatile organic compounds (VOCs) [1]. Presently, E-nose systems have continually been developed to apply in different engineering and industrial areas including food quality analysis, medicine and environmental control etc. In case of food industries applications, the E-nose can be used for detecting the food spoilage [2], identifying the state of freshness [3,4] and monitoring the toxic contamination in beverage [5]. The performance of E-nose is directly related to the different responses of sensors [6]. One of the challenges for the practical food application of E-nose is to detect and distinguish food aromas during cooking processes. If this purpose can be done, the E-nose may be used as a sensing part in robotic chef.

In this work, we have constructed an E-nose and used for the detection of bread baking aromas at four different baking temperatures and four different baking times. Eight metal oxide semiconductor gas sensors were used as sensing part of the E-nose. Percentage changes of sensor responses and principal component analysis (PCA) method have been employed to analyze the data.

### Materials and Methods

#### Bread baking preparation

Fresh bread purchased from a market in Bangkok was baked at four different baking temperatures; 40, 60, 80 and 100 °C, and four different baking times; 5, 10, 15 and 20 minutes. Then, the baked bread was cut into samples with weight about 1-2 g. The samples were placed in the sample bottle for E-nose analysis.

#### E-nose system

The schematic diagram of E-nose system is shown in Fig. 1. It consists of three main components; (I) valves and air pump with mass flow controller, (II) sensor array, and (III) data acquisition (DAQ) & computer. For sensor array, the eight commercial Taguchi gas sensors (TGS) were used as sensing part as listed in Table 1.

Starting, a pump will suck clean air into a mass flow controller. The mass flow controller was used to control air flow rate. In this experiment, the air flow rate was set at 2 L/min. The solenoid valves were used to select the path of aroma molecule delivery. The zero air in the reference bottle was sucked into

sensor array chamber for 5 minutes in order to be a reference line and clear bread baking aromas in sensor chamber. When the sensor responses reached to the resistance baseline, valve 2 was closed and valve 3 was opened. Bread baking aromas in the sample bottle were sucked into sensor array for 1 minute. Then, the resistances of sensors were recorded every 1 minute as a function of time via DAQ for subsequent analysis.

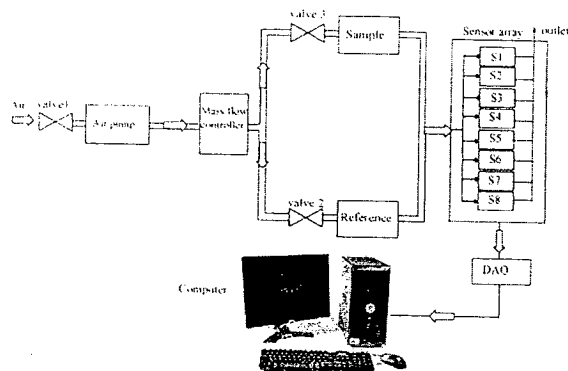


Figure 1. Schematic diagram of E-nose system.

Table 1: Lists of sensor array

Sensor number	Sensor name	Sensing type
S1	TGS 821	Hydrogen
S2	TGS 822	Organic Solvent Vapors
S3	TGS 825	Hydrogen Sulfide
S4	TGS 826	Ammonia
S5	TGS 2600	Air Contaminants
S6	TGS 2602	Air Contaminants
S7	TGS 2610	LP gas
S8	TGS 2620	Solvent Vapors

### Principal component analysis (PCA)

The principal component analysis (PCA) [7,8] was employed for recognition and discrimination of bread baking aromas from measurements of the E-nose system. In principles, PCA process contains five following steps: (I) Get data from matrix, (II) Normalize the data matrix by the mean subtraction, (III) Calculate the covariance matrix, and determine eigenvectors and eigenvalues of the covariance matrix. The calculated eigenvectors must be unit eigenvectors. (IV) Rearrange the eigenvectors and eigenvalues. The eigenvectors are ordered by eigenvalues from highest to lowest. And (V) Obtain the PCA result by matrix multiplication and transpose. The obtained new dataset with orthogonal linear transformation are usually plotted in two or

three dimensions containing the most relevant of the data set.

### Results and Discussion

The resistance changes of each sensor are displayed in Fig. 2. We can be seen that these curves differ from each other in the form of curve shapes and maximum value of resistance changes depending on the type of each sensor. This result shows that all sensors are sensitive to bread baking aromas. The resistances of all sensors decrease when the bread baking aromas are introduced into sensor chamber. It implies that most deoxidizing gases can emit from the bread baking.

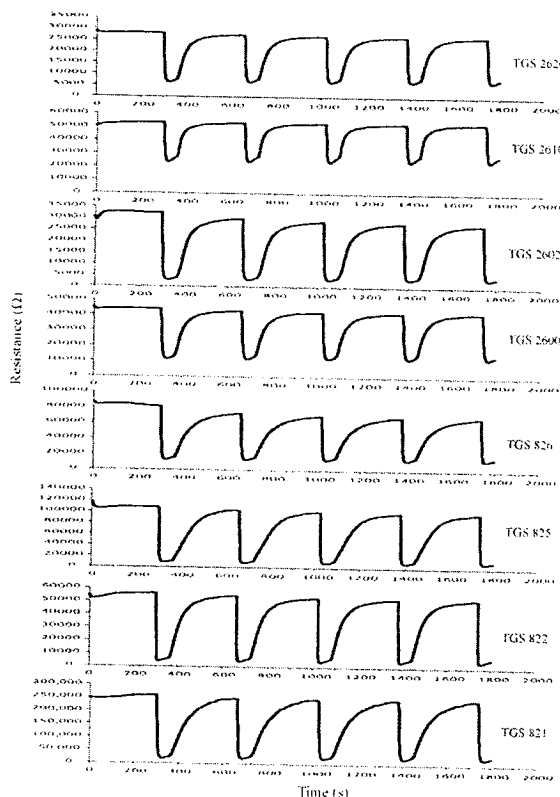


Figure 2. Resistance changes of each sensor as a function of time.

The percentages of sensor responses can be obtained from following equation;

$$\text{Sensor reponse (\%)} = \frac{R_0 - R_{\text{Sens}}}{R_0} \times 100 \quad (1)$$

where  $R_0$  is the value of resistance baseline and  $R_{\text{Sens}}$  is the value of sensitive resistance.

Fig. 3 shows the three dimensional plot of the percentages of sensor responses at different baking temperatures for baking time of 15 min. We can obviously observe that all sensors exhibit high response to the bread baking aromas in the range of

60-95% at all baking temperatures. At baking temperature of 60 °C, all sensors show the highest response. It refers that more VOCs can emits at this temperature. If baking temperature is so high, some VOCs can be lost.

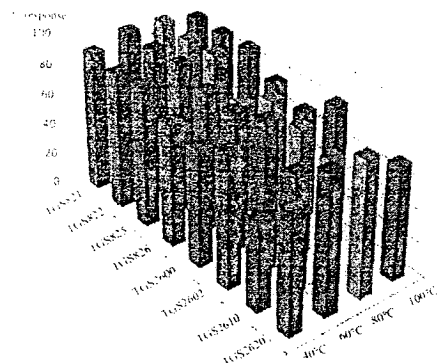


Figure 3. 3D plot of the percentages of sensor response at different baking temperatures.

All data sets were introduced into PCA. Fig. 4 shows the PCA plot of bread baking aromas at different baking temperatures. It can be observed that the PCA plot clearly discriminates the bread baking aromas to four clusters related to different baking temperatures and time. The best result occurs at baking time of 15 min. From results, it suggests that baking time of 15 min can well generate the unique pattern of bread baking aromas at a function of baking temperatures.

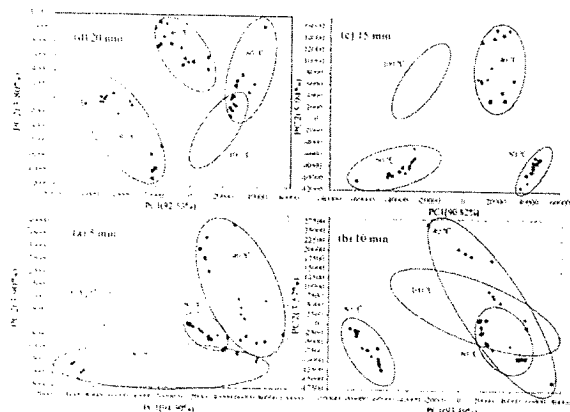


Figure 4. PCA plot of bread baking aromas at (a) 5 min, (b) 10 min, (c) 15 min, and (d) 20 min of baking time with different baking temperatures.

## Conclusions

In this work, an E-nose has been developed for food application during cooking processes. An example has been demonstrated in term of bread baking aromas detection and classification. The TGS sensor array shows high response to bread baking

aromas in the range of 60-95%. With condition of bread baking time at 15 min and baking temperature of 60 °C, the bread product can generate a unique pattern of aroma. Combined with PCA method, our E-nose can classify bread baking aromas at the different bread baking conditions. It is hoped that our E-nose will be installed in robotic chef for real-time monitoring food aroma during cooking processes in near future.

## Acknowledgments

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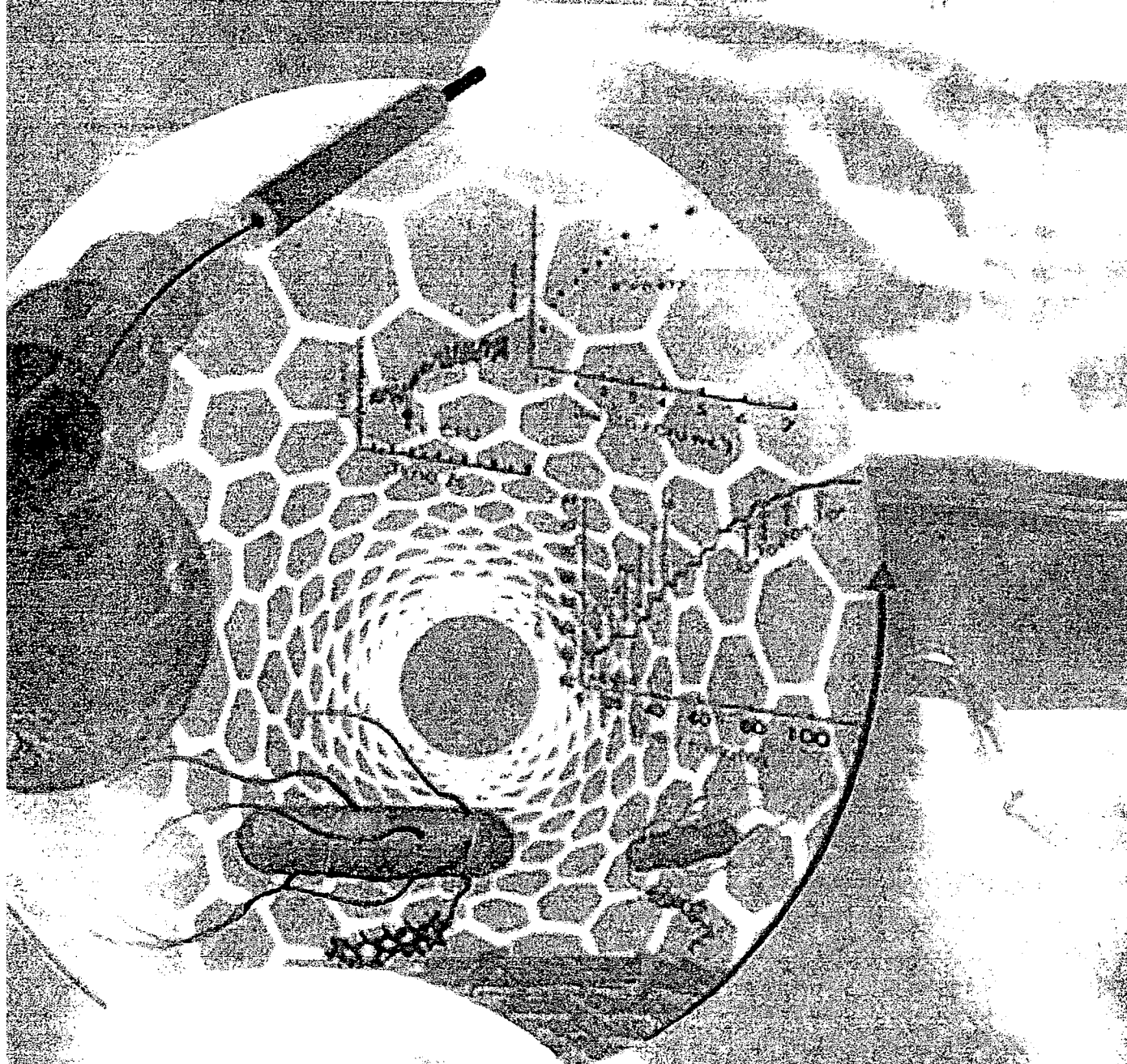
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## Invention of Stereo Electronic Nose for Mobile Robot

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Although human olfactory system is able to discriminate more than 10,000 different odorants, detection of chemicals with high molecular weight (>300 daltons) and various toxic gases are still limited. Nowadays, the gas-sensitive mobile system has become a necessary tool to detect toxic gas and gas leaks in several situations since many gases can highly affect people's health and they are difficult to detect by human nose. In this paper, we have described a design of gas-sensitive system (called as stereo electronic nose) that is suitable for installing on a mobile robot. The stereo electronic nose system consists of four gas sensors including methane CNG gas sensor (MQ-4), LPG gas sensor (MQ-6), flammable gas sensor (MQ-9), and air quality control gas sensor (MQ-135). Such gas sensors were installed at a center of rectangular box. Two fans were set up at sidewalls of box with controllable of the air flow direction by using an electric relay circuit. The stereo electronic nose system has tasted in closed chamber with several gases. The distance between gas sources and stereo electronic nose has been varied from 5-80 cm with many directions in order to investigate the relative equations for identification of the gas leak source. The results show that the stereo E-nose can sense a various types of gases and can identify the direction of gas sources. The gas sensitivity of stereo E-nose decreases when source distance increases. Our stereo E-nose can be used as the olfactory system in a mobile robot for gas source identification.

**Keywords:** Electronic nose, Metal oxide, Semi-conductor gas sensors, Gas source identification

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